

TITLE OF THE INVENTION

ENDOSCOPIC SUTURING SYSTEM

CROSS-REFERENCE TO RELATED APPLICATIONS

5 This is a Continuation-in-Part application of
U.S. Patent Application No. 10/353,866, filed
January 29, 2003, the entire contents of which are
incorporated herein by reference.

This application claims the benefit of
U.S. Provisional Applications No. 60/352,728,
10 filed January 30, 2002; and No. 60/430,259, filed
December 2, 2002.

BACKGROUND OF THE INVENTION

The present invention relates to a treatment
device which can be inserted into a body together with
15 an endoscope. United State Patent No. 5,171,258
(Symbiosis Co., Ltd.) discloses a medical instrument
that is applicable to a surgical operation using a
laparoscope. This medical instrument comprises a pair
of posts for supporting a pair of clevises in order to
20 produce a large force required to grip a thick tissue.
However, the posts and clevises interfere with each
other, whereby an angle that can be formed between the
clevises is restricted to an angle of about 90 degrees.

On the other hand, where the inside of a body
25 is sutured by using an endoscope, it is required to
puncture a needle through a tissue. Therefore, a
treatment device is required to be a small size,

nevertheless the treatment device being capable of moving a needle over a large angle, is required. Further, it is required to transmit a large force to the needle in order to securely puncture the tissue.

5 However, in the prior art, a treatment device for endoscope requiring a large opening/closing angle and transmission of a large force cannot be provided.

BRIEF SUMMARY OF THE INVENTION

10 The present invention has been made in view of the above described circumstance. It is an object of the present invention to provide an endoscopic treatment device comprising a structure for further increasing an opening/closing angle and further producing a large force.

15 According to an aspect of the present invention, there is provided a treatment device which is used to perform treatment in a body by being operated outside the body. This treatment device comprises a flexible member having a distal end portion that can be inserted
20 into a body, a link mechanism which is arranged at the distal end portion of the flexible member and actuated by an operation outside the body, and a curved needle which is actuated by the link mechanism and can move in a direction to puncture a tissue and a direction to be
25 removed from the tissue.

 According to another aspect of the present invention, there is provided an endoscopic treatment

device which is used together with an endoscope to perform treatment in a body by being operated outside the body. This endoscopic treatment device comprises a transmission member with a flexible structure which has
5 a distal end portion inserted into a body and can be operated outside the body, a push rod coupled to the distal end portion of the transmission member, first and second connecting members coupled to the push rod, each of the first and second connecting members having
10 a distal end portion and a proximal end portion rotatably coupled to the push rod, first and second arm members each having a distal end portion and a proximal end portion rotatably coupled to the distal end portion of a corresponding one of the first and second
15 connecting members, a holding member which rotatably holds the distal end portions of the respective arm members at a predetermined interval therebetween, first and second actuating members which are integrally formed with the distal end portions of the arm members
20 and can open/close when the transmission member actuates the first and second connecting members and the first and second arm members through the push rod, and a needle which is mounted on at least one of the first and second actuating members and is used to
25 puncture a tissue.

According to still another aspect of the present invention, there is provided an endoscopic treatment

device which includes recovery means for recovering the thread inserted into a tissue from a needle, wherein the recovery means has a lock member which detaches the needle from one of the first and second actuating members.

According to still another aspect of the present invention, there is provided an endoscopic treatment device comprising recovery means which is used together with an endoscope to recover a thread inserted into a tissue to perform treatment in a body by being operated outside the body, wherein the recovery means has a needle lock member which can lock a needle, and a thread lock member which can lock a thread, thereby forming needle/thread fixing means which can clamp a tissue between the needle locked to the needle lock member and the thread lock member.

According to still another aspect of the present invention, there is provided an endoscopic treatment device comprising a restriction mechanism which is mounted on at least one of first and second actuating members which can open/close, and restricts a movement range of one actuating member.

According to still another aspect of the present invention, there is provided an endoscopic treatment device which is used together with an endoscope to perform treatment in a body by being operated outside the body. This endoscopic treatment device comprises a

transmission member with a flexible structure which has a distal end portion inserted into a body and can be operated outside the body, a push rod coupled to the distal end portion of the transmission member, first
5 and second connecting members coupled to the push rod, each of the first and second connecting members having a distal end portion and a proximal end portion rotatably coupled to the push rod, first and second arm members each having a distal end portion and a proximal
10 end portion rotatably coupled to the distal end portion of a corresponding one of the first and second connecting members, a holding member which rotatably holds the distal end portions of the respective arm members at a predetermined interval therebetween, first
15 and second actuating members which are integrally formed with the distal end portions of the arm members and can open/close when the transmission member actuates the first and second connecting members and the first and second arm members through the push rod,
20 a third actuating member which is pivotally attached to the first actuating member, a third connecting member which is pivotally coupled to the holding member and the third actuating member and moves together with the first and second actuating members, and a needle which
25 is mounted on at least one of the first and second actuating members and is used to puncture a tissue.

According to still another aspect of the present

invention, there is provided a treatment device which is used together with an endoscope to perform treatment in a body by being operated outside the body. This treatment device comprises a needle which is used to
5 puncture a living tissue and to which a thread for suturing the tissue is fixed; a recovery member capable of recovering the needle inserted into the tissue, the recovery member having an outer periphery portion at which a groove is provided and an inner hole; a guide
10 formed in an elongated shape and capable of guiding the recover member; an elongated circular member capable of being inserted into the guide; and at least one arm provided at a distal end of the elongated circular member, wherein the recovery member is engaged with the
15 elongated circular member when the arm and the groove are located in the guide.

According to still another aspect of the present invention, there is provided a treatment device which is used together with an endoscope to perform treatment
20 in a body by being operated outside the body. This treatment device comprises a recovery member capable of recovering a needle punctured into a tissue, the recovery member having an outer periphery portion at which a protrusion is formed; a guide formed in an
25 elongated shape and having an inner hole, the guide being capable of guiding the recovery member; circular members having a distal end portion at which a groove

has been provided, each of which is capable of being inserted into the guide; and another elongated circular member capable of being inserted into the circular member, wherein, when the protrusion and the groove are engaged with each other, the recovery member and the circular members can be integrally advanced and retracted, and the elongated circular member and the circular members can be separated from each other.

According to still another aspect of the present invention, there is provided a treatment device which is used together with an endoscope to perform treatment in a body by being operated outside the body. This treatment device comprises a transmission member with a flexible structure which has a distal end portion inserted into a body and is capable of being operated outside of the body; a push rod coupled to the distal end portion of the transmission member; first and second connecting members coupled to the push rod, each of the first and second connecting members having a distal end portion and a proximal end portion rotatably coupled to the push rod; first and second arm members each having a distal end portion and a proximal end portion rotatably coupled to the distal end portion of a corresponding one of the first and second connecting members; a holding member which rotatably holds the distal end portions of the first and second arm members; first and second actuating members which are

integrally formed with the distal end portions of the first and second arm members and are able to open/close when the transmission member actuates the first and second connecting members and the first and second arm members through the push rod; a needle which is mounted at least at one of the first and second actuating members and is used to puncture a tissue; a thread mounted on the needle; and a recovery member capable of recovering the needle, wherein one of the first and second actuating members has a loop portion, and the recovery member can pass through the loop.

According to still another aspect of the present invention, there is provided a treatment device which is used together with an endoscope to perform treatment in a body by being operated outside the body. This treatment device comprises a transmission member with a flexible structure which has a distal end portion inserted into a body and is capable of being operated outside of the body; a push rod coupled to the distal end portion of the transmission member; first and second connecting members coupled to the push rod, each of the first and second connecting members having a distal end portion and a proximal end portion rotatably coupled to the push rod; first and second arm members each having a distal end portion and a proximal end portion rotatably coupled to the distal end portion of a corresponding one of the first and second connecting

members; a holding member which rotatably holds the distal end portions of the first and second arm members; first and second actuating members which are integrally formed with the distal end portions of the first and second arm members and are able to open/close when the transmission member actuates the first and second connecting members and the first and second arm members through the push rod; a needle which is mounted at least at one of the first and second actuating members and is used to puncture a tissue; a thread mounted on the needle; a recovery member capable of recovering the needle; and an operating member having a cylindrical outer periphery portion at which a groove has been formed and a central axis, wherein the operating member can operate the recovery member via the groove when the operating member rotates around the central axis.

According to still another aspect of the present invention, there is provided a suturing method using an endoscopic suturing device. This method comprises:

(1) retaining an insert assisting device into a body;

(2) inserting a suturing device incorporated in the endoscope into the insert assisting device and inserting the suturing device into the body;

(3) opening a curved needle of the suturing device;

(4) pushing the curved needle against a sutured region;

(5) puncturing the curved needle into a tissue;

5 (6) recovering the needle by using a recovery member;

(7) removing the curved needle from the tissue;

(8) moving the recovery member close to the sutured region; and

10 (9) returning the recovery member to a predetermined position, and removing the suturing device to the outside of the body by closing the curved needle.

Advantages of the invention will be set forth in the description which follows, and in part will be
15 obvious from the description, or may be learned by practice of the invention. Advantages of the invention may be realized and obtained by means of the instrumentalities and combinations particularly pointed out hereinafter.

20 BRIEF DESCRIPTION OF THE SEVERAL VIEWS OF THE DRAWING

The accompanying drawings, which are incorporated in and constitute a part of the specification, illustrate embodiments of the invention, and together with the general description given above and the
25 detailed description of the embodiments given below, serve to explain the principles of the invention.

FIG. 1 is an illustrative view showing an entire

configuration of an endoscopic suturing system according to a first embodiment of the present invention;

FIG. 2 is an enlarged view of an endoscope and
5 a suturing device shown in FIG; 1;

FIG. 3 is an illustrative view showing a state in which first and second actuating members of the suturing device are closed;

FIG. 4 is an illustrative view showing a state in
10 which the first and second actuating members of the suturing device are opened;

FIG. 5 is a sectional view showing an internal structure of the suturing device of FIG. 3;

FIG. 6 is a sectional view showing an internal
15 structure of the suturing device of FIG. 4;

FIG. 7 is a sectional view taken along the line A-A of FIG. 5;

FIG. 8 is a view seen in a direction indicated by the arrow B of FIG. 4;

FIG. 8A is a view showing a suturing device when
20 an endoscope is removed, the view being similar to FIG. 8;

FIG. 9 is a sectional view taken along the line C-C of FIG. 7;

FIG. 10 is a sectional view taken along the line
25 D-D of FIG. 7;

FIG. 11 is a sectional view taken along the line

E-E of FIG. 7;

FIG. 12 is a sectional view taken along the line F-F of FIG. 13;

FIG. 13 is a view seen in a direction indicated by the arrow G of FIG. 7;

FIG. 14 is a view showing a hook of a thread-catching-device when a suture thread is hooked;

FIG. 15 is a view showing a hook of a thread-catching-device when the suture thread and hook are retracted into a sheath;

FIG. 15A is a view showing an outer appearance of another thread-catching-device;

FIG. 15B and FIG. 15C are views showing how the thread-catching-device catches a thread by using a hook;

FIG. 16 is a schematic longitudinal cross section of an insert assisting device;

FIG. 17 is an illustrative view showing a state in which an endoscope having a suturing device mounted thereon is housed in an insert assisting device;

FIG. 18 is an illustrative view showing a state in which the endoscope having the suturing device mounted thereon is protruded from the insert assisting device;

FIG. 19 is a view showing a modified example of a valve mounted on the insert assisting device;

FIG. 20 is a view showing the insert assisting device according to a modified example when the

endoscope and the suturing device are mounted;

FIG. 21 is a view showing a state in which the endoscope and the suturing device are protruded from the insert assisting device of FIG. 20;

5 FIG. 22 to FIG. 27 each show a suturing procedure using the suturing device, wherein FIG. 22 is a view showing a state in which a curved needle is proximal to a tissue;

10 FIG. 23 is a view showing a state in which the curved needle punctures a tissue;

FIG. 24 is a view showing a state in which the thread-catching-device hooks the suture thread;

15 FIG. 25 is a view showing a state in which the suture thread is retracted into a flexible tubular member together with the hook when the thread is hooked;

FIG. 26 is a view showing a state in which the thread-catching-device is pulled out from an instrument channel port;

20 FIG. 27 is a view showing a state in which the curved needle is removed from the tissue;

FIG. 28 is a view showing a state in which the suturing device is removed from the cavity together with the insert assisting device;

25 FIG. 29 is a view showing a state in which a knot is fed into a body by using a knot pusher;

FIG. 30 is a view showing a state in which the

suturing device is housed in a protect member, the figure being similar to FIG. 2 showing an endoscopic suturing system according to a second embodiment of the present invention;

5 FIG. 31 is an illustrative view showing a state in which the suturing device is protruded in the endoscopic suturing system of FIG. 30;

 FIG. 32 to FIG. 35 are views each showing a protect member in the second embodiment, wherein
10 FIG. 32 is a view showing a state in which a movable portion is protruded;

 FIG. 33 is a view showing a state in which a moving member disengages a lock member;

 FIG. 34 is a view showing a state in which
15 the movable portion is retracted;

 FIG. 35 is a detailed view of the lock member;

 FIG. 36 is an illustrative view of the protect member using an endoscopic suturing system according to a third embodiment of the present invention;

20 FIG. 37 to FIG. 41 each show an endoscopic suturing system according to a fourth embodiment, wherein FIG. 37 is a view showing a suturing device used therefor;

 FIG. 38 is a view showing a state in which
25 a removable needle after punctured into a tissue is engaged with a needle thread fixing device;

 FIG. 39 is a view showing a state in which

an injury is closed by tying the suture thread;

FIG. 40 is a view showing a state in which a redundant portion of the suture thread is cut by a thread cutting device;

5 FIG. 41 is a sectional view taken along the line H-H of FIG. 37;

FIG. 42 is a sectional view showing a state in which sealing means is incorporated into the frontal side of the insert assisting device shown in FIG. 16;

10 FIG. 43 is a sectional view taken along the line I-I of FIG. 42;

FIG. 44 is a view showing a suturing device for use in an endoscopic suturing system according to a fifth embodiment of the present invention;

15 FIG. 45 is a view showing a state in which a removable needle after punctured into a tissue is engaged with a needle thread fixing device;

FIG. 46 is a view showing a suturing device for use in an endoscopic suturing system according to a sixth embodiment of the present invention;

20 FIG. 47 is a view showing a state in which a removable needle after punctured into a tissue is engaged with a needle fixing device;

FIG. 48 is a view showing a state in which a knot is formed by a loop removed from an engagingly lock member when the first and second actuating members are opened;

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FIG. 49 is a view showing a state in which a redundant portion of the suture thread is cut by a thread cutting device;

FIG. 50 is a view showing a state in which
5 a tissue is sutured while the tissue is pulled by a grasping forceps;

FIG. 51 is a view showing a state for use in an endoscopic suturing system according to a seventh embodiment of the present invention;

10 FIG. 52 is a view showing a state when a removable needle after punctured into a tissue is engaged with a needle thread fixing device;

FIG. 53 is a sectional view taken along the line J-J of FIG. 52;

15 FIG. 54 is a view showing a structure by thread lock means;

FIG. 54A to FIG. 54D are views showing various modifications of the lock means;

FIG. 55 is a view showing a state in which
20 a needle holder is removed from a tissue;

FIG. 56 is a view showing a state in which a tissue is tied;

FIG. 57 to FIG. 63 each show a suturing procedure using an endoscopic suturing system according to
25 an eighth embodiment of the present invention, wherein FIG. 57 is a view showing a state in which the suturing device is proximal to a tissue to be sutured;

FIG. 58 is a view showing a state in which a removable needle after punctured into a tissue is engaged with a needle fixing device;

FIG. 59 is a view showing a state in which
5 a needle holder is pulled out from a tissue;

FIG. 60 is a view showing a state in which the suturing device and endoscope are spaced from a tissue while the needle thread fixing device is left;

FIG. 61 is a view showing a state in which
10 a tissue is tied with the suture thread;

FIG. 62 is a view showing a state in which the suture thread can be separated;

FIG. 63 is a view showing a state in which a redundant portion of the suture thread is cut by
15 a thread cutting device;

FIG. 64 is a view showing a suturing device for use in an endoscopic suturing system according to a ninth embodiment of the present invention;

FIG. 65 is a view showing a state in which
20 a removable needle after punctured into a tissue is engaged with a needle fixing device;

FIG. 66 is a view showing a tissue when the tissue is sutured;

FIG. 67 to FIG. 99 each show the 10th embodiment, wherein FIG. 67 is a sectional view taken along the
25 line A-A of FIG. 68;

FIG. 68 is a view showing an outer appearance of

a suturing device (a view taken in the direction of an arrow B in FIG. 67);

FIG. 69 is a view taken in the direction of an arrow C in FIG. 67 (with a partially sectional view);

5 FIG. 70 is a view taken in the direction of an arrow D in FIG. 69;

FIG. 71 is a sectional view taken along the line E-E of FIG. 69;

10 FIG. 72 is a sectional view taken along the line F-F of FIG. 69;

FIG. 73 is a sectional view taken along the line G-G of FIG. 69;

FIG. 74 is a view showing the details of the operating section of the suturing device;

15 FIG. 75 is a sectional view taken along the line H-H of FIG. 74;

FIG. 76 is a view showing an outer appearance of a pre-knot cartridge;

20 FIG. 77 to FIG. 80 are views for explaining how a removable needle is removed by using a needle-catching-device;

FIG. 81 to FIG. 85 are views showing how the removable needle is removed by using the needle-catching-device;

25 FIG. 86 and FIG. 87 are views showing a state wherein a cover is so mounted as to prevent a pre-knot of the pre-knot cartridge from coming off the

needle-catching-device;

FIG. 88 is a view showing an outer appearance of a spring for locking the removable needle mounted in the needle-catching-device;

5 FIG. 89 is a view showing in detail how a pre-knot is formed;

FIG. 90 to FIG. 98 are views showing a suturing procedure;

FIG. 99 is a view showing a needle-catching-sheath
10 as another modification of the needle-catching-sheath;

FIG. 100 to FIG. 111 each show the 11th embodiment, wherein FIG. 100 is view showing an outer appearance of a suturing device (a view taken in the direction of an arrow G in FIG. 102);

15 FIG. 101 is a partially sectional view of FIG. 100;

FIG. 102 is a sectional view taken along the line A-A of FIG. 100;

FIG. 103 is a view taken in the direction of
20 an arrow B in FIG. 101;

FIG. 104 is a sectional view taken along the line C-C of FIG. 101;

FIG. 105 is a sectional view taken along the line D-D of FIG. 101;

25 FIG. 106 is a sectional view taken along the line E-E of FIG. 102;

FIG. 107 is a sectional view taken along the line

F-F of FIG. 102;

FIG. 108 to FIG. 111 are views showing how the suturing device punctures the tissue;

FIG. 112 to FIG. 122 each show the 12th
5 embodiment, wherein FIG. 112 is a view showing an outer appearance of a suturing device (a view taken in the direction of an arrow G in FIG. 114);

FIG. 113 is a partially sectional view of
FIG. 112;

10 FIG. 114 is a sectional view taken along the line A-A of FIG. 112;

FIG. 115 is a view taken in the direction of an arrow B in FIG. 113;

15 FIG. 116 is a sectional view taken along the line C-C of FIG. 113;

FIG. 117 is a sectional view taken along the line E-E of FIG. 114;

FIG. 118 is a sectional view taken along the line F-F of FIG. 114;

20 FIG. 119 to FIG. 122 are views showing how the suturing device punctures the tissue;

FIG. 123 to FIG. 126B each show the 13th embodiment, wherein FIG. 123 to FIG. 126A are views showing how the suturing device punctures the tissue;

25 FIG. 126B is a sectional view of the suturing device;

FIG. 127 to FIG. 128B each show the 14th

embodiment, wherein FIG. 127 is a view showing a method of fixing a scope and a suturing device;

FIG. 128A is a sectional view of a tube holder;

FIG. 128B is a view showing an arrangement
5 obtained by mounting a protecting member in the arrangement shown in FIG. 127;

FIG. 129 to FIG. 143 each show the 15th embodiment, wherein FIG. 129 to FIG. 141 are views showing a procedure for continuously suturing the
10 tissue;

FIG. 142 and FIG. 143 are views showing how a continuous suturing operation is performed;

FIG. 144 to FIG. 163 each show the 16th embodiment, wherein FIG. 144 is a partially sectional
15 view of a suturing device;

FIG. 145 is a sectional view taken along the line A-A of FIG. 144;

FIG. 146 is a partial sectional view of an end loop cartridge in FIG. 158;

FIG. 147 to FIG. 157 are views showing the
20 operation of a suturing device when puncturing the tissue;

FIG. 158 is a view showing an outer appearance of the end loop cartridge;

FIG. 159 is a view showing an outer appearance of
25 a lock tubular member;

FIG. 160 and FIG. 161 are views showing a seal

structure and operating section formed on the proximal end side of the suturing device;

FIG. 162 is a sectional view of the distal end portion of a thread cutting forceps used to cut
5 a suture thread;

FIG. 163 is a view showing another example of the structure of an outer sheath;

FIG. 164 is a view showing a state wherein the end loop cartridge is loaded in a suturing device;

10 FIG. 165 and FIG. 166 are views showing another form of a removable needle;

FIG. 167 is a view showing a state wherein the suturing device is mounted on an endoscope and the distal end of the suturing device is brought nearest to
15 the distal end of the endoscope;

FIG. 168 is a view showing a state wherein the distal end of the suturing device is separated from the distal end of the endoscope;

FIG. 169 to FIG. 171 each show the 17th embodiment, wherein FIG. 169 is a partial sectional
20 view showing a state wherein the first and second actuating members of a suturing device are open;

FIG. 170 is a partially sectional view showing a state wherein the first and second actuating members
25 of the suturing device are closed;

FIG. 171 is a sectional view taken along the line A-A of FIG. 169;

FIG. 172 is a view showing a state wherein the tissue is punctured with a suturing device according to the 18th embodiment;

FIG. 173 and FIG. 174 are views showing a
5 modification of a needle holder which can applied to the 10th embodiment;

FIG. 175 and FIG. 176 are views showing another modification of the needle holder;

FIG. 177 is a view showing a fixing needle which
10 can applied to the 10th embodiment and other embodiments;

FIG. 178 and FIG. 179 each show the 19th embodiment, wherein FIG. 178 is a view showing a state wherein an end loop cartridge is to be mounted in an
15 engage tube, and FIG. 179 is a view showing a state wherein the end loop cartridge is mounted in the engage tube;

FIG. 180 and FIG. 181 each show the 20th embodiment, wherein FIG. 180 is a view showing a state
20 wherein an end loop cartridge is to be mounted in an engage tube, and FIG. 181 is a view showing a state wherein the engage tube and a hood device are housed in a distal pipe;

FIG. 182A to FIG. 190 each show a twenty-first
25 embodiment of the present invention, wherein FIG. 182A is an illustrative view showing a state before an end loop cartridge is assembled with a suturing device;

FIG. 182B is an illustrative view showing an engagingly lock member of FIG. 182A;

FIG. 182C is an illustrative view showing the engagingly lock member and a circular member in an exploded manner;

FIG. 183 is a sectional view showing a state in which the end loop cartridge is housed in a guide member of the suturing device;

FIG. 184 is a sectional view showing a state in which the end loop cartridge is engaged with a removable needle;

FIG. 185 and FIG. 186 are sectional views showing a variety of end loop cartridges;

FIG. 187 is a view showing an outer appearance of the end loop cartridge;

FIG. 188A is an illustrative view showing a state in which the removable needle punctures a tissue;

FIG. 188B is an illustrative view showing a state in which the end loop cartridge is engaged with the removable needle;

FIG. 188C is an illustrative view showing a state in which the end loop cartridge removes the removable needle from a needle holding member;

FIG. 188D shows the needle holding member that has been pulled from the tissue;

FIG. 188E depicts the suture thread 442 that is pulled via the hook 463 to tie up the tissue;

FIG. 188F shows the lock member 458 opened or closed as the end loop cartridge 440 is moved to the left in the drawing by using the lock member 458 and ring-shaped member 681;

5 FIG. 189 illustrates the end loop cartridge that has been removed from the lock member;

FIG. 190 is an illustrative view when the end loop cartridge is removed from the engagingly lock member;

10 FIG. 191 is a sectional view similar to FIG. 183, showing a twenty-second embodiment of the present invention;

FIG. 192A to FIG. 195 each show a twenty-third embodiment of the present invention, wherein FIG. 192A is an illustrative view showing a state before an end
15 loop cartridge is assembled with a suturing device;

FIG. 192B is a view showing an outer appearance of the end loop cartridge;

FIG. 193 is an illustrative view showing a state in which the end loop cartridge is housed in a guide
20 member;

FIG. 194 is a longitudinal sectional view of FIG. 193;

FIG. 195 is an illustrative view showing a state in which the end loop cartridge is removed from an
25 engagement device;

FIG. 196 to FIG. 199 each show a twenty-fourth embodiment of the present invention, wherein FIG. 196

is a longitudinal sectional view similar to FIG. 194;

FIG. 197 is an illustrative view showing a state before an end loop cartridge is mounted on an engagement member;

5 FIG. 198 is a perspective view of the state shown in FIG. 197;

FIG. 199 is a sectional view showing a state in which the end loop cartridge is pushed inwardly from the state shown in FIG. 197;

10 FIG. 200 is a view showing an outer appearance of a hook used in the sixteenth and twenty-first embodiments;

FIG. 201 shows a twenty-fifth embodiment of the present invention and is a view showing an outer
15 appearance of a hook compared with that of FIG. 200;

FIG. 202 to FIG. 208 each show a twenty-sixth embodiment of the present invention, wherein FIG. 202 is a view showing a state in which a suturing device is assembled with an endoscope;

20 FIG. 203 is a sectional view showing a state in which the suturing device is allocated in an insert assisting device;

FIG. 204 is a sectional view showing a state in which the suturing device is protruded from the insert
25 assisting device to the outside;

FIG. 205 is an illustrative view showing a state in which the endoscope is passed through an air tight

valve;

FIG. 206 is an illustrative view showing a state in which a band for further enhancing air tightness is wound from the state shown in FIG. 205;

5 FIG. 207 is a sectional view taken along the line A-A of FIG. 206, showing a state before the band is mounted;

 FIG. 208 is a sectional view taken along the line A-A of FIG. 206, showing a state in which the band has
10 been mounted;

FIG. 209 and FIG. 210 each show a twenty-seventh embodiment of the present invention, and are a plan view and a side view of an operating section which can be applied to the sixteenth or twenty-first embodiment;

15 FIG. 211 is a partial sectional view of FIG. 209;

 FIG. 212 is a view showing an outer appearance of a knob shown in FIG. 211;

 FIG. 213 is an exploded view showing a groove formed at an outer periphery portion of the knob shown
20 in FIG. 212;

FIG. 214 is a view similar to FIG. 209, showing an operating section according to a twenty-eighth embodiment of the present invention;

 FIG. 215A and FIG. 215B are detailed views each
25 showing a scope holder shown in FIG. 202;

 FIG. 216 is an illustrative view showing a state in which the operating section and scope holder are

engaged with each other;

FIG. 217 to FIG. 223C each show a twenty-ninth embodiment of the present invention, wherein FIG. 217 and FIG. 218 are partial sectional views each showing a scope holder;

FIG. 219 and FIG. 220 are illustrative views each showing a state in which a suturing device has been mounted on an endoscope;

FIG. 221 is a view showing an outer appearance of a protrusive and recessed handle and a protrusive and recess pipe of the scope holder;

FIG. 222 is a view showing a part of an outer appearance of the scope holder shown with a plurality of tubes in their twisted state;

FIG. 223A is a view showing a part of an outer appearance of the scope holder shown with a plurality of tubes in their bent state;

FIG. 223B is a view showing the entire device for use in the twenty-first embodiment;

FIG. 223C is a view taken in the direction of an arrow A in FIG. 223B;

FIG. 224 to FIG. 225B each show a thirtieth embodiment of the present invention, wherein FIG. 224 is an illustrative view showing a state in which an endoscope is mounted on a suturing device;

FIG. 225A is a view showing a state in which a jig is fixed to a scope fixing portion;

FIG. 225B is an illustrative view showing a field of view of the endoscope when the jig is used;

FIG. 226 shows a thirty-first embodiment of the present invention, and is an illustrative view showing a state in which an endoscope has been mounted on a suturing device;

FIG. 227 and FIG. 228 each show a thirty-second embodiment of the present invention, wherein FIG. 227 is an illustrative view showing a state in which an endoscope is mounted on a suturing device;

FIG. 228 is an illustrative view comparatively showing a state in which a scope fixing portion is unstable;

FIG. 229 to FIG. 231 each show a thirty-third embodiment of the present invention, wherein FIG. 229 is a view showing a field of view of an endoscope in a state in which a removable needle is mounted on a needle holding member;

FIG. 230 is a view showing a field of view of the endoscope in a state in which the removable needle has been mounted from the needle holding member;

FIG. 231 is an illustrative view showing an end loop cartridge with a mark;

FIG. 232 to FIG. 234 each show a thirty-fourth embodiment of the present invention, wherein FIG. 232 is an illustrative view showing a part of a suturing device;

FIG. 233 is an illustrative view showing the suturing device having a second active member formed in a loop shape;

FIG. 234 is a view showing a relationship between
5 the active member of FIG. 233 and the end loop cartridge;

FIG. 235 shows a thirty-fifth embodiment, and is a sectional view showing a suturing device;

FIG. 236A to FIG. 237C each show a thirty-sixth
10 embodiment of the present invention, wherein FIG. 236A is an illustrative view showing a needle holding member and a removable needle;

FIG. 236B and FIG. 236C are sectional views each showing the removable needle and a thread fixing
15 portion;

FIG. 237A is an illustrative view showing a needle holding member and a removable needle according to a modified example;

FIG. 237B and FIG. 237C are views similar to
20 FIG. 236B and FIG. 236C, respectively.

FIG. 238 is a sectional view showing the end loop cartridge according to the twenty-first embodiment; and

FIG. 239 shows a thirty-seventh embodiment, and is a sectional view showing a state in which a center line
25 of thread lock means allocated in an end loop cartridge has been displaced.

DETAILED DESCRIPTION OF THE INVENTION

[First Embodiment]

FIG. 1 to FIG. 29 show an endoscopic suturing system according to a first embodiment of the present invention. In the respective systems described hereinafter, although the endoscopic suturing system is used, a gripping forceps, a scissors forceps, a hot biopsy forceps, or a rotational clipping device may be used instead of the suturing system.

As shown in FIG. 1, an endoscopic suturing system 1 according to the present embodiment comprises an endoscope system 2, a suturing device 3, and a suture thread 4. This suture thread 4 is preferably formed like a monofilament line or stranded wire by using a material such as nylon, polyester, silk, fluoroplastic or bioabsorbable resin. The endoscope system 2 comprises an endoscope 12, an image processing device 14, a light source device 15, an observation monitor 13, and a suction device 11 as in a generally used videoscope system. The endoscope 12 is connected to the light source device 15 via a universal code. Then, an image signal delivered from a CCD camera 10 (refer to FIG. 8) at its distal end portion is processed in the image processing device 14, and the processed image is displayed on the monitor 13. As best shown in FIG. 2, although the endoscope 12 is used as having an instrument channel port 6, an

endoscope of such type having two instrument channel ports may be used instead thereof.

5 In addition, as shown in FIG. 8, the CCD camera 10, light guides 8 and 9, instrument channel port 6, and lens washing nozzle 11 for the CCD camera are arranged at a distal end portion of the endoscope 12. A fiberscope with its eyepiece lens may be used instead of the videoscope using the CCD. As shown in FIG. 8, although the suturing device 3 is removably fixed at
10 a distal end of the endoscope 12 by a fixing member 40, the suturing device 3 and the endoscope 12 may be structured integrally with each other instead thereof.

As shown in FIG. 3 to FIG. 7, the suturing device 3 comprises a flexible tube 73 described later and
15 a holding member 18 fixed at its distal end portion to hold a needle described later. This holding member 18 is formed of: two support plate portions 18a opposed to each other through a slit 31 (refer to FIG. 7); and a hole 19 (refer to FIG. 5) which communicates with
20 the slit 73 between these support plate portions and an inner hole of the flexible tube 73. In this hole 19, a push rod 20 is disposed retractably in an axial direction.

At a distal end of this push rod 20, one end of
25 each of first and second connecting members 22 and 23 is pivoted via a pin 21. The other end of each of the connecting members 22 and 23 is pivoted at a proximal

end portion of each of first and second arm members 24 and 25 via pins 26 and 27, respectively. Further, a first actuating member 16 formed integrally with the first arm member 24 is rotatably linked with the support plate portion 18a via a pin 28. Similarly, a second actuating member 17 formed integrally with the second arm member 25 is rotatably linked with the support plate portion 18a via a pin 29.

In FIG. 7, as is illustrated by the pin 28, the pins 28 and 29 each have an end portion formed by a reduced diameter portion 30. In this manner, the size of the slit 31 defined between the support plate portions 18a of the holding member 18 is maintained to be slightly larger than a sum of the thickness of the first actuating member 16 and the second actuating member 17. The first actuating member 16 and the second actuating member 17 can be moved in the slit 31 without generating a remarkable friction.

As shown in FIG. 7, the push rod 20 is linked with an elongated flexible transmission member 71. In addition, the holding member 18 is linked with coils 72 and 76 that form an axial hole. These coils 72 and 76 are linked with each other at their end faces opposed to each other by suitable means such as laser welding, blazing, soldering, adhering or the like. The coil 76 is formed of an element wire that is more smaller in diameter than the coil 72, whereby the

suturing device 3 is formed more flexibly at its distal end side. These coils 72 and 76 are covered with the flexible tube 73 almost all over their full lengths, and is held so as to be in intimate contact with this
5 flexible tube 73. The tube 73 restricts contraction in the axial direction of the coils 72 and 76, thereby increasing a force for opening and closing the first actuating member 16 and the second actuating member 17.

As shown in FIG. 2, frontal side end portions of
10 the tube 73 and the coil 72 are fixed to an operating member main body 77 of an operating member 67 of the suturing device. In addition, a frontal side end portion of the transmission member 71 is inserted into the operating member main body 77, and is linked with
15 a pipe 74 while it is inserted into the pipe 74 that is slidable relative to this operating member main body 77. This pipe 74 is connected to a movable member 75 by a link member (not shown). Therefore, when the movable member 75 is moved relative to the operating
20 member main body 77, the first actuating member 16 and the second actuating member 17 can be opened/closed via the transmission member 71.

As shown in FIG. 5 and FIG. 6, the first and second arm members 24 and 25 can pass through the pins
25 28 and 29, and can be opened up to an angle shown in FIG. 6. The length of these first and second arm members 24 and 25 each and the length of the first and

second connecting members 22 and 23 each are properly set, whereby an angle between the first and second arm members 24 and 25 can be further increased or decreased, of course. Needless to say, these members
5 can be opened/closed within the angle range of 95 degrees or more and less than 360 degrees.

As shown in FIG. 7 and FIG. 11, a stopper pin 32 is fixed to the push rod 20. The stopper pin 32 is guided to the inside of a slit 33 that extends in
10 a longitudinal direction formed at the holding member 18, as shown in FIG. 3, FIG. 4, and FIG. 7, and the movement in the opening direction of the first and second actuating members 16 and 17 can be restricted.

A curved needle 34 is fixed to a distal end of the
15 first actuating member 16. Alternatively, this curved needle 34 may be detachably mounted on the first actuating member 16. A needle eye 5 into which a suture thread 4 can be inserted is formed at a distal end side of the curved needle 34. In addition, as
20 shown in FIG. 8, the curved needle 34 is so small in thickness as to be better punctured into a tissue.

As shown in FIG. 5 to FIG. 8A, the second actuating member 17 has bifurcated fixing arms 43 and 44. Fixing needles 41 and 42 are fixed to distal ends
25 of these fixing arms 43 and 44, respectively. In the present invention, although the fixing needles 41 and 42 are fixed integrally to the fixing arms 43 and 44,

these needles may be removably mounted. On the other hand, as shown in FIG. 7, a protect member 45 having holes 46 and 47 formed thereat is fixed to the first actuating member 16 by screws 48 and 49. As shown in
5 FIG. 5 and FIG. 6, this protect member 45 covers a needle tip of the fixing needles 41 and 42 each when the first and second actuating members 16 and 17 are closed. For example, this protect member prevents a tissue or the like from being caught by the fixing
10 needles 41 and 42. Alternatively, the protect member 45 may have a structure in which a recess 254 is formed in a first actuating member 218 as in the 10th embodiment (see FIG. 68) (to be described later).

As shown in FIG. 5 and FIG. 11, a channel member
15 35 is fixed to the holding member 18 via an L shaped supporting member 39. This channel member 35 has: a pipe 36 formed of a comparatively hard member disposed at its distal end portion; and a tube 37 formed of a comparatively soft material tightened by a fixing
20 thread 38 after pressed into this pipe. This fixing thread 38 is fixed to the tube 37 by an adhesive. This pipe 36 is inserted into a concave portion 52 (refer to FIG. 11) of the support member 39, and is fixed to this support member 39 by proper means such as
25 brazing, soldering, or bonding. This support member 39 is formed of two elongated holes 53 through which screws 50 and 51 can pass, as shown in FIG. 11 and

FIG. 13, whereby the support member 39 can be fixed to the holding member 18 by the screws 50 and 51 so as to make it possible to adjust a position relevant to the holding member 18.

5 In addition, as shown in FIG. 10 and FIG. 11, a protect member 54 is fixed to the pipe 36 by proper means such as brazing, soldering, or bonding. This protect member 54 covers a needle tip of the curved
10 needle 34 when the first and second actuating members 16 and 17 are closed, and prevents the curved needle 34 from being caught by a tissue or the like. As shown in FIG. 11 and FIG. 13, a thread guide 55 having its axial hole through which the suture thread 4 can pass is mounted on the support member 39. This thread guide 55
15 is composed of: a pipe 57 formed of a relatively hard material; and a tube 58 formed of a relatively soft material. The pipe 57 is fixed to the tube 58 by proper means such as press-in or bonding, for example. In addition, the pipe 57 is fixed to the support member
20 39 by proper means such as brazing, soldering, or bonding.

 As shown in FIG. 11 to FIG. 13, like the thread guide 55, a thread guide 56 is fixed to the holding member 18 by screws 62 and 63. This thread guide 56
25 is composed of: a pipe 59 formed of a relatively hard material; a tube 60 formed of a relatively soft material; and a plate shaped support member 61.

The support member 61 and the pipe 59 are fixed by appropriate means such as brazing, soldering, or bonding.

As shown in FIG. 2, the tube 37 communicates with
5 a base 64 linked with the operating member main body 77 at its frontal side. A biopsy valve 69 is attached to the frontal side of this base 64. In addition, tubes 58 and 60 communicate with holes 65 and 66 formed at the operating member main body 77, respectively, at
10 their frontal side.

In addition to the above described fixing member 40 (refer to FIG. 8), the suturing device 3 according to the present embodiment is fixed at several positions to an insert portion 7 of the endoscope 12 by another
15 fixing member 70 as shown in FIG. 2. These fixing members 70 as well are removably formed, whereby the suturing device 3 can be removably mounted on the insert portion 7 of the endoscope 12. Of course, the suturing device 3 and the insert portion 7 are formed
20 integrally with each other, whereby they are made removable from each other.

As shown in FIG. 2, FIG. 14, and FIG. 15, a thread-catching-device 68 for catching the suture thread 4 comprises: a hook 79 which is movable in
25 an axial direction and rotatable within a flexible tubular member 78 formed of a coil or the like; and an operating member 80 of the thread-catching-device for

operating the hook 79. The hook 79 advances and retracts a grip 81 disposed movably via a pipe 83, for example, whereby the hook can be housed in the flexible tubular member 78 or can be protruded therefrom. The
5 suture thread 4 can slid on this hook 79 when it is hooked by the hook 79. In addition, a stopper 82 which inhibits advancing movement of the grip 81 is engaged in the pipe 83, for example, whereby the hook 79 can be locked so as not to come off the flexible tubular
10 member 78. Such a thread-catching-device 68 is formed to have outer diameter capable of passing through the inside of the channel 35. Alternatively, a thread-catching-device 524 shown in FIG. 15A to FIG. 15C may be used. This thread-catching-device 524
15 has a hook 525 on which the suture thread 4 can slide as in the case with the thread-catching-device 68. In addition, a guide member 526 is so formed as to face the thread-catching-device 524. As shown in FIG. 15C, the curved needle 34 is caught between the guide member
20 526 and the hook 525 to facilitate catching the suture thread 4 by using the hook 525.

FIG. 16 shows an insert assisting device 84 for inserting the insert portion 7 that includes the suturing device 3 into a body.

25 The insert assisting device 84 according to the present embodiment comprises: a flexible tubular member 85 formed in a shape such that its distal end

can be easily inserted into a body, for example, in a tapered shape; two valves 86 and 87 having circular holes 90 and 91 disposed respectively at the proximal end side of this flexible tubular member 85; and a base 89 which communicates with an axial hole of the flexible tubular member 85. This base 89 can be used to connect an aspirator (not shown) via a tube, for example, if an aspirating function is required. It is preferable that this base 89 be sealed with a cap (not shown) when it is not used.

As shown in FIG. 19, instead of the above described valves 86 and 87, a plurality of slits 94 are provided around a hole 93, thereby making it possible to use a valve 92 such that an object having its external diameter larger than the hole 93 can pass.

In addition, instead of the insert assisting device 84, an insert assisting device 95 shown in FIG. 20 and FIG. 21 may be used. This insert assisting device 95 comprises: a flexible tubular member 96; a flexible hood member 97 disposed frontally of the flexible tubular member 96; and a fixing member 98 for fixing this hood member so as to be almost sealed at the insert portion 7 that includes the suturing device 3. This insert assisting device 95 is useful to maintain air tightness in a body. After this insert assisting device 95 has been inserted into the body, an endoscope is pushed out in a direction indicated by the

arrow in FIG. 21, whereby the suturing device 3 fixed to this endoscope can be protruded from the flexible tubular member 96.

In addition, as shown in FIG. 42 and FIG. 43,
5 sealing means 144 may be provided at the proximal end side of the suturing device 3 and the endoscope 12.

This sealing means 144 comprises: an inner tube 140 having its inner diameter through which the endoscope 12 can pass; and an outer tube 141 having
10 its inner diameter larger than the inner tube 140, the outer tube having this inner tube inserted therethrough. The outer diameter of the outer tube 141 is slightly larger than the inner diameter of each of the holes 90 and 91 of the valves 86 and 87. Tubes 37,
15 58, 60, and 73 and the like are passed through a space formed between the inner tube 140 and the outer tube 141. A sealing member 142 is filled in a space between these tubes. At both ends of the inner tube 140, a space between the tube and the endoscope 12 is sealed
20 by a tape 143. In this manner, a space between the insert assisting device 84 and the suturing device 3 and the endoscope 12 are securely sealed, and air is fed into a body, thereby preventing air leakage when the body is inflated.

25 Now, suturing procedures using the above described suturing system will be described here.

(1) The suturing device 3 and the endoscope 12

assembled in a state shown in FIG. 2 are inserted into the flexible tubular member 85 shown in FIG. 16, and are disposed until a state shown in FIG. 17 has been obtained. At this time, the suture thread 4 is
5 inserted into the needle eye 5 of the curved needle 34, and each end portion passes through the thread guides 55 and 56 each. Then, the suture thread 4 is held so as to be pulled out of the suturing device 3 from the holes 65 and 66 of the operating member main body 77.
10 In addition, the endoscope 12 is connected to the image processing device 14, the light source device 15 and the like (FIG. 1) via a universal code. Then, while the inside of the body is observed through the monitor 13, the flexible tubular member 85 having the suturing
15 device 3 and the endoscope 12 housed therein is inserted into a required location in the body.

(2) The inside of the body is inflated by using an air feeding function such as an endoscope, thereby providing a space.

20 (3) As shown in FIG. 18, the endoscope 12 is advanced, whereby the suturing device 3 is protruded from the flexible tubular member 85.

(4) The suturing device 3 is placed close to the suture site, the movable member 75 shown in FIG. 2 is
25 pushed, and the second actuating members 16 and 17 are opened as shown in FIG. 4.

(5) As shown in FIG. 22, the movable member 75 is

operated while the curved needle 34 and the fixing needles 41 and 42 are pushed against the suture site. As shown in FIG. 23, the first and second actuating members 16 and 17 are closed.

5 (6) As shown in FIG. 24, the suture thread 4 coming off a tissue is hooked by the hook 79 of the thread-catching-device 68 inserted via the biopsy valve 69. As shown in FIG. 25, the suture thread 4 is retracted into the flexible tubular 78 together with
10 the hook 79.

 (7) As shown in FIG. 26, the thread-catching-device 68 is pulled out from the channel 35 to the outside of the body, and the suture thread 4 is pulled out from the biopsy valve 69. At this time, the suture
15 thread 4 slides on the hook 79, whereby one end portion of the suture thread 4 moves from one of the thread guides 55 and 56 into the channel 35, and is pulled out from the channel 35 to the outside of the body together with the thread-catching-device 68. The other end
20 portion of the suture thread 4 is held so as to be inserted through the other end of the thread guides 55 and 56 each.

 (8) As shown in FIG. 27, the movable member 75 is operated, the first and second actuating members 16 and
25 17 are opened, and the curved needle 34 and the fixing needles 41 and 42 are pulled out from a suture site.

 (9) As shown in FIG. 28, the suturing device 3 is

retracted again into the flexible tubular member 85, and the suturing device 3 is pulled out from the inside of the cavity together with the flexible tubular member 85.

5 (10) A knot is formed in the suture thread 4 at the outside of the body, and this knot is fed into the body several times by the knot pusher 99 as shown in FIG. 29. The knot pusher 99 shown in FIG. 29 has a hood shaped cylindrical member mounted on a distal end
10 portion of the endoscope, and two holes are provided on a side face of this cylindrical member. Of course, any knot pusher is available for use without being limited to the shown knot pusher 99 as long as it has
15 a structure or form such that a knot can be fed into the body. In addition, for example, a knot itself such as Grinch knot or Loaders knot may be formed movably. In this case, the knot can be fed into the body by using proper means.

 (11) Lastly, an endoscope on which the suturing
20 device 3 is not mounted is inserted into an endoscope, and a residual suture thread 4 is cut by using a scissors forceps or the like.

 According to the endoscopic suturing system 1 of the present embodiment, the first and second actuating
25 members 16 and 17 holding the curved needle 34 and the fixing needles 41 and 42 are formed integrally with the first and second arm members 24 and 25 that can be

pass through the pins 28 and 29, whereby a large opening/closing angle can be formed between the first and second actuating members 16 and 17. In this manner, even in a size which is small for an endoscope, there can be formed a suturing device having one or a plurality of needles capable of moving all over a sufficiently large angle required for a suturing operation.

In addition, the coils 72 and 76 linked with the holding member 18 that rotatably supports the first and second actuating members 16 and 17 are restricted from expansion and contraction by the flexible tube 73. Thus, a large force can be transmitted via the coils 76 and 72. In this manner, a large force required for a suturing operation can be transmitted to needles 34, 41, and 42 via the coils 76 and 72 and the first and second actuating members 16 and 17.

Further, the suturing device 3 is fixed to the insert portion of the endoscope 12, thereby making it easily to do a suturing work by a flexible endoscope that has been very difficult in the prior art.

Furthermore, a minimal invasive suturing procedure can be carried out for a patient because no open surgical operation is required.

As described above with reference to each of the above embodiments, when the tissue is to be sutured, for example, a grasping forceps 152 is inserted into

the body through the instrument channel port 6 of the endoscope 12, as shown in FIG. 50. While the tissue is pulled by this grasping forceps 152, the first and second actuating members 16 and 17 can be closed, and
5 the tissue can be punctured with a curved needle 34. The subsequent procedure is the same as that described with reference each of the embodiments.

[Second Embodiment]

FIG. 30 to FIG. 35 each show an endoscopic
10 suturing system according to a second embodiment of the present invention. A variety of endoscopes described hereinafter are basically similar to those according to the above described embodiment. Like elements are designated by like reference numerals. A detailed
15 description thereof is omitted here.

As shown in FIG. 30 and FIG. 31, a system according to the present embodiment comprises a protect member 100 mounted at a distal end portion of the insert portion 7 of the endoscope 12, the protect
20 member 100 covering the distal end portion of the suturing device 3. This protect member 100 comprises: a cylindrical fixing portion 104, for example, that can be removably fixed at a distal end of the insert portion 7; and a movable portion 103 slidably mounted
25 on the outer periphery of this fixing portion 104. This movable portion 103 is preferably made of a transparent resin, e.g., polycarbonate, norbornene

resin, cycloolefin-based resin, or polyethylene terephthalate.

As shown in FIG. 32 to FIG. 34, at a wall portion of the fixing portion 104, there are formed an axial
5 hole 111 and radial holes 113 and 114 having this axial hole communicating with a peripheral face at the proximal part of each end portion. In addition, at the outer periphery of the fixing portion 104, a lock member 106 shown in FIG. 35 is fixed with screws or the
10 like inserted via mount holes 118 and 119, for example. This lock member 106 comprises engaging portions 116 and 117 which is disposed so as to be almost perpendicular relative to the outer periphery face of the fixing portion when fixed to the fixing portion
15 104, and an inclined portion 115 which descends gradually toward a distal end from a space between these engaging portions. The entirety of the lock member is formed of a resilient material such as metal or resin. At a position that corresponds to
20 these engaging portions 116 and 117 each, an opening 112 is formed at the outer periphery face of the fixing section 104. In this manner, when the lock member is compressed against the outer periphery face of the fixing portion 104, the engaging portions 116 and 117
25 are housed in the opening 112, and the entirety of the lock member 106 is flattened.

On the other hand, the movable portion 103 has:

a concave portion 120a defined at its distal end side on an engaging wall 120 which can be engaged with the engaging portions 116 and 117 of the lock member 106; and a concave portion 108a communicating with this
5 concave portion 120a, the concave portion being limited at its distal end side on an engaging wall 108. The rear end side of these concave portions 108a and 120a each is defined by the engaging wall 109. In the concave portion 108a, there are housed an inclined
10 portion 115 of the lock member 106; and a moving member 107 that controls engagement or disengagement between this lock member 106 and the engaging wall 120.

The moving member 107 according to the present embodiment is formed of a hard material, for example,
15 in a substantially cylindrical shape or flat shape. It is preferable that its length be formed to be larger than the axial dimension of the concave portion 120a and be formed so as to be housed in the concave portion 108a without compressing the inclined portion 115 when
20 the engaging portions 116 and 117 and the engaging wall 120 are engaged with each other. Transmission members 105 and 121 are extended, respectively, from an end portion of this moving member 107. The transmission member 105 is extended from the concave portion 120a
25 via a small hole that passes through the engaging wall 109. The transmission member 121 is extended to the inner periphery side of the movable portion 103 from

a slit 110 that communicates with the concave portion 108a, and further, is extended to the outer periphery of the fixing portion via a radial hole 113, an axial hole 111, and a radial hole 114 of the fixing portion 104. These transmission members 105 and 121 extend to the operating member main body 77 shown in FIG. 30 and FIG. 31 via a proper flexible tube (not shown), and is connected with operating member 101 and 102 of the protect member 100.

In this protect member 100, movement in the right side on paper of the movable portion 103 is restricted when an engagingly lock wall formed at the movable portion 103 as shown in FIG. 32 abuts against the engaging portions 116 and 117 of the lock member 106 fixed to the fixing portion 104. In this manner, as shown in FIG. 30, the needle fixed to the distal end portion of the suturing device is covered with the movable section 103, and is free of being exposed to the outside.

If the operating member 101 of the protect member 100 connected to the transmission member 105 is pulled in this state, the moving member 107 moves in the right direction, as shown in FIG. 33. At this time, the moving member 107 rolls over the inclined portion 115 of the lock member 106, and thus, the engaging portions 116 and 117 are housed in the opening 112, and are disengaged from the engaging wall 120. The movable

portion 103 can move to the rear end side, i.e., to the right side shown in the figure. Further, when the operating member 101 of the protect member 100 is pulled, the moving member 107 abuts against the engaging wall 109, as shown in FIG. 34, and the movable portion 103 moves to the right side together with the moving member 107 and enters a state shown in FIG. 31. At this time, the lock member 106 abuts against the inner periphery face at both sides of the slit 110 formed at the movable portion 103. In contrast, if the operating member 102 of the protect member 100 connected to the frontal side of the transmission member 121 is pulled, the movable member 107 moves to the left side, and is engaged with the engaging wall 108. Then, the movable portion 103 moves to the left side together with the moving member 107. If the engaging wall 120 exceeds the opening 112, the lock member 106 returns to a state shown in FIG. 32 by its resilience. Then, the engaging portions 116 and 117 are protruded again from the outer periphery face of the fixing portion 104, whereby the movement in the left direction of the movable portion 103 can be restricted.

Now, the suturing procedure using the above described suturing system will be described here.

(1) The above described protect member 100 is mounted on the suturing device and endoscope assembled

as in the above described embodiment, and then, the operation member 102 of the protect member 100 is pulled. In this manner, the moving portion 103 is protruded at its distal end side and comes into a state shown in FIG. 30. In this state, the moving portion is inserted into the body while the inside of the body is observed through the endoscope 12.

(2) After insertion into the body, the operating member 101 of the protect member 100 is pulled, and the moving portion 103 is retracted to enter a state shown in FIG. 31. In this manner, a distal end portion of the suturing device 3 is exposed so that a suturing operation can be carried out by using a procedure similar to that according to the first embodiment.

(3) After suturing has been completed, the moving portion 103 is protruded in a state shown in FIG. 30 by pulling the operating member 102 of the protect member 100. In this state, the suturing device and endoscope is removed from the body.

In the present embodiment, the moving portion 103 of the protect member 100 moves in an axial direction. Thus, the outer diameter of the device can be reduced in addition to advantageous effect of the first embodiment. Furthermore, operation can be simplified.

[Third Embodiment]

FIG. 36 shows a protect member 122 used for an endoscopic suturing system according to a third

embodiment of the present invention.

The protect member 122 according to the present embodiment comprises: a fixing portion 124 fixed to a distal end portion of an insert portion 7; and
5 a movable portion 123 that can slide on this fixing portion 124. An externally sealed annular space 128 is formed between these fixing portion and movable portion. A base 125 communicating with the annular space 128 is mounted at the outer periphery of the
10 movable portion 123, a fluid 127 can be poured into or discharged from the annular space 128. This fluid 27 may be liquid or gas.

In the present embodiment, at the protect member 122, for example, when the suitable fluid 127 such
15 as physiological saline, water, or air is filled in a fluid pouring device (not shown) such as syringe, and this fluid is poured into the annular space 128, the movable portion 123 slides to the right side on paper. In contrast, the fluid 127 is discharged from
20 the annular space 128 by setting a fluid pouring device 129 to a negative pressure, the movable portion 123 can slide to the left side.

Advantageous effect similar to each of the above described embodiments is provided by using this protect
25 member 122.

[Fourth Embodiment]

FIG. 37 to FIG. 41 each show an endoscopic

suturing system according to a fourth embodiment of the present invention.

As shown in FIG. 37, in the present embodiment, a needle holder 132 is fixed to a first actuating member 16 of a suturing device 3, and a removable needle 131 is removably connected to a distal end of the needle holder 132. This removable needle 131 has a shaft portion 138, and one end of a suture thread 130 is fixed to a distal end of the shaft portion 138. The needle holder 132 has a groove 137 opened along almost all the full length at the inner periphery side, as shown in FIG. 41, and the suture thread 130 is removably extended inside of the groove 137.

On the other hand, the other end of this suture thread 130 extends to the frontal vicinity of the endoscope through thread lock means 135 formed at a needle thread fixing device 133. This thread lock means 135 is formed so that the suture thread 130 can be moved arbitrarily in a direction indicated by the arrow B, i.e., in a direction in which the suture thread is retracted. In contrast, the lock means 135 is formed so that the suture thread cannot be moved in a direction indicated by the arrow A, i.e., in a direction in which the suture thread is advanced.

Further, as shown in FIG. 38, needle lock means 134 capable of engaging a removable needle 131 as well is formed at the needle thread fixing device 133.

It is preferable that this needle lock means 134 be formed of a resilient member or the like. In the present embodiment, this needle thread fixing device 133 is removably mounted on a distal end of a needle fixing device main body 139. This needle thread fixing device main body 139 can be inserted into a body via a suitable channel 35. In addition, although the needle thread fixing device 133 is engaged by being pressed into the needle thread fixing device main body 139, the fixing device can be fixed to be grasped by a suitable device such as a grasping forceps, for example.

In this case, the removable needle 131 and needle thread fixing device 133 described above are at least partly made of a biocompatible metal such as stainless steel, pure titanium or titanium alloy, a biocompatible resin such as polyimide, poly(etheretherketone) (PEEK), polysulfon, liquid crystal polymer, or polyamide, a biocompatible ceramic material such as alumina, silicon nitride, or the like. As in the first embodiment, the suture thread 130 is formed like a monofilament line or stranded wire by using a material such as nylon, polyester, silk, fluoroplastic or bioabsorbable resin.

This endoscopic suturing system can be used as follows.

(1) The suturing device 3 is inserted into a body while its distal end portion is protected by the insert assisting devices 84 and 95 according to the first

embodiment described above; a protect member 100 according to the second embodiment; or alternatively, a protect member 122 or the like according to the third embodiment. The inside of the body can be observed
5 through the endoscope 12 as in the above described embodiment.

(2) During suturing, the first actuating member 16 and the second actuating member 17 are closed so as to press the removable needle 131 and the fixing needles
10 41 and 42 against a suture site, and the removable needle 131 is punctured into a tissue.

(3) As shown in FIG. 38, the removable needle 131 after punctured is protruded from the tissue. Thereafter, the removable needle 131 is inserted into
15 the needle lock means 134 of the needle thread fixing device 133 by pushing out the needle fixing device main body 139 toward the front end side, and is latched thereby.

(4) When the first actuating member 16 and the
20 second actuating member 17 are opened, the removable needle 131 is latched by the needle lock means 134. Thus, the removable needle 131 is removed from the needle holder 132, and the suture thread 130 is removed from the groove 137 of the needle holder 132. In this
25 manner, as shown in FIG. 39, the suture thread 130 remains in the tissue while a portion between the needle thread fixing device 133 and thread lock means

135 forms a loop.

(5) As shown in FIG. 39, the needle thread fixing main body 139 is advanced toward the tissue while an end portion of the suture thread 130 disposed at the outside of the body is pulled frontally. In this manner, a loop of the suture thread 130 is contracted, and the tissue is tied until a state shown in FIG. 40 has been obtained.

(6) Lastly, a redundant suture thread 130 is cut by a thread cutting device 136. The needle thread fixing device 133 left in the body can be removed during thread removal.

According to the system of the present embodiment, in addition to advantages according to the above described first and second embodiments, there is no need for making a knot outside of the body, and feeding the knot into the body. This makes it possible to reduce an operation time, and further, facilitate procedures. In addition, the tied state of the tissue can be easily adjusted.

[Fifth Embodiment]

FIG. 44 and FIG. 45 each show a fifth embodiment of the present invention. This fifth embodiment is basically similar to the above-described fourth embodiment, and is different therefrom in the point below.

As shown in FIG. 44, the needle thread fixing

device 133 according to the present embodiment is removable mounted on a holding member 145 formed at the second actuating member 17.

5 The needle thread fixing device 133 described above are at least partly made of a biocompatible metal such as stainless steel, pure titanium or titanium alloy, a biocompatible resin such as polyimide, poly(etheretherketone) (PEEK), polysulfon, liquid
10 crystal polymer, or polyamide, a biocompatible ceramic material such as alumina, silicon nitride, or the like.

 This endoscopic suturing system can be used as follows.

 (1) When the suturing device 3 is inserted into a body, its distal end portion is particularly
15 protected by the insert assisting devices 84 and 95, protect member 100, protect member 122 or the like according to the above described embodiment, for example. The needle thread fixing device 133 is
20 mounted on the second actuating member 17, thus making it unnecessary to use a thread fixing device main body 139 or an ordinary grasping forceps and the like, for example.

 (2) During suturing, as in the fourth embodiment, the first actuating member 16 and the second actuating
25 member 17 are closed so as to press the removable needle 131 and fixing needles 41 and 42 against a suture site, and the removable needle 131 is punctured

into a tissue.

(3) As shown in FIG. 45, the removable needle 131 protruded from a tissue after punctured is inserted into the needle lock means 134 of the needle thread fixing device 133 held at the holding member 145, and is engaged therewith.

(4) When the proximal end side of the suture thread 130 is pulled, the tissue is tied because one end of the suture thread 130 is fixed to the removable needle 131, and the groove 137 of the needle holder 132 is opened at the inner periphery side.

(5) When the first actuating member 16 and the second actuating member 17 are opened, the removable needle 131 is engaged with the needle lock means 134. Thus, the removable needle 131 and the needle thread fixing device 133 are removed from the holding member 145 to enter a state shown in FIG. 40.

(6) Lastly, a redundant suture thread 130 is cut by the thread cutting device 136.

In the present invention, advantages similar to those according to the fourth embodiment are obtained. Further, in the present embodiment, there is no need for holding the needle thread fixing device 133 solely, and thus, the suturing operation is further facilitated.

[Sixth Embodiment]

FIG. 46 to FIG. 49 each show a sixth embodiment.

The sixth embodiment as well is basically similar to the fourth embodiment, and is different therefrom in the point below.

As shown in FIG. 46, in the present embodiment,
5 four engagingly lock members 146 for holding at least one loop formed in advance at the suture thread 130 made of the same material as that in the first embodiment are provided at the second actuating member 17. These engagingly lock members 146 are formed of a
10 resilient element in a claw shape, and is fixed so that two of these lock members are opposed to the remaining two members at a site opposed to the first actuating member 16. A part of the suture thread 130 is hooked by these engagingly lock members 146, and two large
15 loops 148, for example, are formed. The removable needle 131 can pass through the inside of these large loops 148. Further, at least one loop 149 for forming a knot described later is formed at the periphery of the suture thread 130 that forms the large loop 148 and
20 a knot like a pre-knot 232 shown in, for example, FIG. 89 (to be described later) is formed.

A needle fixing device 150 comprises: needle fixing means 147 capable of being engaged with the removable needle 131; and a tubular member 151 to which
25 this needle fixing means is fixed. This needle fixing device 150 is formed so that the device can be inserted into a suitable channel 35. Alternatively, the needle

fixing device 150 may be fixed onto the suturing device
3. In this case, a position at which the needle fixing
device 150 corresponds to a position at which the
removable needle 131 can be engaged with the needle
fixing means 147.

This endoscopic suturing system can be used as
follows.

(1) When the suturing device 3 is inserted into
a body, as in the above described embodiment, the
device is protected by the above described insert
assisting devices 84 and 95, protect member 100,
a protect member 122 or the like, for example.

(2) When the removable needle 131 is punctured
into a tissue, the first actuating member 16 and the
second actuating member 17 are closed so as to press
the removable needle 131 and the fixing needles 41 and
42 against a suture site.

(3) As shown in FIG. 47, the removable needle 131
after punctured is protruded from the tissue.
Thereafter, the tubular member 151 is pushed out toward
the front end side, the removable needle 131 is
inserted into the needle lock means 147 of the needle
thread fixing device 150 held on the tubular member
151, and is latched thereby.

(4) As shown in FIG. 48, when the first actuating
member 16 and the second actuating member 17 are
opened, the removable needle 131 is engaged with the

needle engagingly lock means 147. Thus, the removable
needle 131 is removed from the needle holder 132, and
a large loop 148 is removed from the engagingly lock
member 146. In this manner, a small loop 149 forms
5 a knot on a suture thread 130 in corporation with the
large loop.

(5) Then, as shown in FIG. 49, the proximal end
side of the suture thread 130 and the needle fixing
device 150 are pulled, the knot 149 is tied, and an
10 injury is sutured.

(6) Lastly, as shown in FIG. 49, a redundant
suture thread 130 is cut by a thread cutting
device 136.

This system according to the sixth embodiment
15 provides advantages that are similar to those according
to the above described fourth embodiment. In addition,
there is no need for keeping any member except the
suture thread 130 in the body.

As has been described with respect to each of the
20 above described embodiments, when a tissue is sutured,
a grasping forceps 152, for example, can be inserted
into a body through the instrument channel port 6 of
the endoscope 12 as shown in FIG. 50. While the tissue
is pulled by this grasping forceps 152, the first and
25 second actuating members 16 and 17 are closed, thereby
making it possible to puncture the removable needle 131
into the tissue. The subsequent procedure is similar

to that described with respect to the respective embodiments.

[Seventh Embodiment]

FIG. 51 to FIG. 56 each show a seventh embodiment
5 of the present invention. In this system, a structure
of the suturing device 3 is different from that
according to the above described fourth embodiment.
Further, a needle thread fixing device 153 is disposed
instead of the needle thread fixing device 133 in the
10 above described embodiment.

As shown in FIG. 51, the needle thread fixing
device 153 comprises thread lock means 155 and needle
lock means 154. This thread lock means 155 is composed
of a resilient tubular member having its small axial
15 hole, and the suture thread 156 is inserted into this
axial hole so as to be pressed into the hole. In this
manner, the thread lock means 155 can engagingly lock
the suture thread 156 at an arbitrary position. This
thread lock means 155 can be formed of a silicon tube
20 or the like, for example. On the other hand, in the
case where sufficient strength cannot be obtained by
a silicon tube which is easily broken after ligation,
for example, a reinforce member 200 such as a PTFE
resin based tube may be disposed coaxially of the
25 thread lock means 155, as shown in FIG. 54.

In addition, the thread lock means 155 may be
modified into a thread lock means 565 as shown in

FIG. 54A. The thread lock means 565 is comprised of an elastic member 566 and tubular member 567. The tubular member 567 is arranged on the outer surface of the elastic member 566 and has at least one recess formed by an outer force to increase the sliding resistance between the thread 156 and the elastic member 566. This makes it possible to increase the tying force in a suturing operation. FIG. 54B to FIG. 54D show arrangements in which the tubular member 567 are deformed in different manners. FIG. 54B shows an arrangement in which a plurality of recesses are formed in the tubular member 567 in the longitudinal direction. FIG. 54C shows an arrangement in which a recess is formed in a direction perpendicular to the longitudinal direction of the tubular member 567. FIG. 54D shows an arrangement in which the tubular member 567 is swaged to uniformly and radially apply a pressure to the elastic member 566.

For the suture thread 156, a loop portion 158 is formed at the proximal end of the suture thread 156. This loop portion 158 is removably engaged with an engaging portion 163. This engaging portion 163 is fixed to a transmission member 165, and is arranged retractably in a coil 164. The proximal end portion of the transmission member 165 is linked with an operating member (not shown) which is operable at the outside of the body. This operating member is advanced or

retracted, whereby the engaging portion 163 can be advanced or retracted along the coil 164. In addition, a channel 160 through which the coil 164 is inserted has a flexible tubular member 162 and a receiving
5 portion 161 fixed to a distal end thereof. A needle thread fixing device 153 is held via this receiving portion 161.

As shown in FIG. 53, an inclined portion 167 is formed at needle lock means 154. In addition, an
10 inclined portion 169 is formed similarly at a removable needle 157 as well. Thus, the needle lock means 154 and the removable needle 157 are hardly removed from each other while they are engaged with each other via these inclined portions 167 and 169. In addition, in
15 the present embodiment, there is provided a through hole 170 opened on a tapered face at a distal end through an axial portion of the removable needle 157. This through hole 170 is formed to have a stepped structure. As shown in FIG. 53, for example, a knot
20 166 formed at the other end of the suture thread 156 is housed in this through hole 170, and this knot 166 can be engaged at a stepped portion so as not to move to the other end side. For this suture thread 156, this knot 166 can be fixed to the removable needle 157 by
25 a suitable bonding agent. In addition, a groove 168 similar to that shown in FIG. 41 is formed at a needle holder 159 that holds this removable needle 157, a

groove 168 similar to that shown in FIG. 41 is formed, and a suture thread 156 can be removed from the needle holder 159.

5 The removable needle 157 and needle thread fixing device 153 described above are at least partly made of a biocompatible metal such as stainless steel, pure titanium or titanium alloy, a biocompatible resin such as polyimide, poly(etheretherketone) (PEEK), polysulfon, liquid crystal polymer, or polyamide, a
10 biocompatible ceramic material such as alumina, silicon nitride, or the like. As in the first embodiment, the suture thread 156 is formed like a monofilament line or stranded wire by using a material such as nylon, polyester, silk, fluoroplastic or bioabsorbable resin.

15 This endoscope suture system can be used as follows.

 (1) When the suturing device 3 is inserted into a body, the suturing device 3 is inserted while its distal end portion is particularly protected as in the
20 above described embodiment.

 (2) The first actuating member 16 and the second actuating member 17 are closed so as to press the removable needle 157 and the fixing needles 41 and 42 against a suture site, and the removable needle 157 is
25 punctured into a tissue. Of course, this operation can be observed through the endoscope 12.

 (3) As shown in FIG. 52, the needle 157 protrudes

from a tissue. Then, the coil 164 is pushed out to the forward side, the removable needle 157 is inserted into needle lock means 154 of the needle thread fixing device 153, and is latched therewith.

5 (4) When the first actuating member 16 and the second actuating member 17 are opened, the removable needle 157 is engaged with the needle lock means 154. Thus, the removable needle 157 is removed from the needle holder 159 to enter a state shown in FIG. 55.

10 (5) A transmission member 165 is pulled to the proximal end side by an operating member (not shown), and a tissue is tied until a state shown in FIG. 56 has been obtained. Then, a distal end portion of the transmission member 165 is protruded from the coil 164,
15 and the loop portion 158 is removed from the engaging portion 163.

 (6) Lastly, a redundant thread 156 is cut by a thread cutting device 136.

 This system according to the seventh embodiment as
20 well provides advantages similar to those according to the above described fourth embodiment. Further, in the present embodiment, a length of the suture thread 156 may be short. Thus, a suturing operation is further facilitated.

25 [Eighth Embodiment]

Embodiment

FIG. 57 to FIG. 63 each show an endoscopic

suturing system according to an eighth embodiment of the present invention.

As shown in FIG. 57, a needle thread fixing device 171 is removably attached to a second actuating member 17 instead of the holding member 145 according to the fifth embodiment (refer to FIG. 44). Needle fixing means 177 is formed at the needle thread fixing device 171. One end of a suture thread 172 is fixed to this needle thread fixing device 171. In addition, the other end of this suture thread is extended into a coil 164 via thread lock means 173 similar to that according to the seventh embodiment, and a loop section 174 is formed.

A needle holder 178 that holds the removable needle 175 at its distal end portion is fixed to a first actuating member 16. One end of the other suture thread 176 is fixed to this removable needle 175, the other end of this suture thread as well is extended in the coil 164 via thread lock means 173, and a loop portion 174 is formed. These loop portions 174 are engaged with an engaging portion 163 of a transmission member 165 as in the seventh embodiment.

A suturing operation using this endoscope system is carried out as follows.

(1) As in the above described embodiments each, the suturing device 3 is inserted into a body while its distal end portion is particularly protected by the

insert assisting devices 84 and 95, protecting member 100, protect member 122 or the like.

(2) As shown in FIG. 58, the first and second actuating members 16 and 17 are closed so as to press
5 the removable needle 175 and the fixing arms 41 and 42 against a suture site, and the removable needle 175 is punctured into a tissue.

(3) As shown in FIG. 58, the removable needle 175 after punctured is inserted into needle fixing means
10 177 of the needle thread fixing device 171 held at a predetermined position, and is engaged therewith.

(4) As shown in FIG. 59, when the first and second actuating members 16 and 17 are opened, the needle
fixing device 171 is removed from the second actuating
15 member 17 while the removable needle 175 is engaged with the needle fixing device 171.

(5) The transmission member 165 is pulled by an operating member (not shown) in a state shown in FIG. 60, a tissue is tied by the suture thread 176
20 until a state shown in FIG. 61 has been obtained. Then, as shown in FIG. 62, a distal end portion of the transmission member 165 is pushed out from the coil 164. The loop portion 174 is removed from the engaging portion 163 of the transmission member. Only the loop
25 portion 174 of one suture thread can be pulled if necessary.

The removable needle 157 and needle thread fixing

device 171 described above are at least partly made of a biocompatible metal such as stainless steel, pure titanium or titanium alloy, a biocompatible resin such as polyimide, poly(etheretherketone) (PEEK), polysulfon, liquid crystal polymer, or polyamide, a biocompatible ceramic material such as alumina, silicon nitride, or the like. As in the first embodiment, the suture thread 172 is formed like a monofilament line or stranded wire by using a material such as nylon, polyester, silk, fluoroplastic or bioabsorbable resin.

(6) Lastly, as shown in FIG. 63, redundant suture threads 172 and 176 are cut by the thread cutting device 136.

This system according to the eighth embodiment as well provides advantages similar to the above described fourth embodiment. Further, in the present embodiment as well, a length of the suture threads 172 and 176 each may be short. Thus, a suturing operation is further facilitated.

[Ninth Embodiment]

FIG. 64 to FIG. 66 each show an endoscopic suturing system according to a ninth embodiment of the present invention. The ninth embodiment is different from the eighth embodiment in the point below.

As shown in FIG. 64, in the present embodiment, a first actuating member 190 is disposed at needle holders 179 and 180 each mounting removable needles 184

and 185 each. A groove opened inwardly is extended at these needle holders 179 and 180 each, as shown in FIG. 41. In addition, one of the suture threads 186 and 187 each is fixed to the two removable needles 184 and 185 each in a manner similar to the seventh embodiment.

A needle fixing device 181 is removably mounted on the second actuating member 191. Needle lock means 182 and 182 for engaging the removable needles 184 and 185 are formed at the needle fixing device 181.

As shown in FIG. 65, the other ends of the suture threads 186 and 187 are extended into the coil 164 via thread lock means 188 similar to the thread lock means 155 according to the seventh embodiment, and a loop portion 189 is formed. This loop portion 189 as well is engaged with the engaging portion 163 of the transmission member 165 as in the seventh embodiment.

The removable needles 184 and 185 and needle thread fixing device 181 described above are at least partly made of a biocompatible metal such as stainless steel, pure titanium or titanium alloy, a biocompatible resin such as polyimide, poly(etheretherketone) (PEEK), polysulfon, liquid crystal polymer, or polyamide, a biocompatible ceramic material such as alumina, silicon nitride, or the like. As in the first embodiment, the suture threads 186 and 187 are formed like a monofilament line or stranded wire by using a

material such as nylon, polyester, silk, fluoroplastic or bioabsorbable resin.

A suturing operation using this endoscope system is carried out as follows.

5 (1) As in the above described embodiments each, the suturing device 3 is inserted into a body while its distal end portion is protected by the insert assisting devices 84 and 95, protect member 100, protect member 122 or the like as in the above described embodiments
10 each.

 (2) The first and second actuating members 190 and 191 are closed so as to press the needle lock means 182 and 183 and the removable needles 184 and 185 against a suture site, and the removable needles 184 and 185
15 are punctured into a tissue.

 (3) As shown in FIG. 65, the removable needles 184 and 185 after punctured is inserted into the needle lock means 182 and 183 of the needle fixing device 181 held at a predetermined position, and is engaged
20 therewith.

 (4) When the first and second actuating members 190 and 191 are opened, the removable needles 184 and 185 are engaged with the needle fixing device 181. Thus, the removable needle 184 and 185 are removed from
25 the needle holders 179 and 180. In addition, the needle fixing device 181 as well is removed from the second actuating member 191. In this manner, a state

shown in FIG. 65 is obtained.

(5) Then, as in the seventh embodiment, thread lock means 188 is pushed against a tissue, an engaging portion 163 is pulled via the transmission member 165, and the tissue is tied. Then, the engaging portion 163 is pushed out from the coil 164, and the loop portion 189 is removed.

(6) Lastly, redundant suture threads 186 and 187 are cut by the thread cutting device 136 as in the fourth embodiment.

On the other hand, as shown in FIG. 66, the tying force may be adjusted with a length of one suture thread 192 instead of the two suture threads 186 and 187. In this case, measures such as thread lock means 188, the engaging portion 163, the coil 164, the transmission member 165, the loop portion 189 and the like become unnecessary.

This system according to the ninth embodiment as well provides advantages similar to the above described fourth embodiment. Further, in the present embodiment, the two suture threads 186 and 187 can be sutured at the same time by the two removable needles 184 and 185. [10th Embodiment]

FIG. 67 to FIG. 99 show the 10th embodiment. (Arrangement)

The 10th embodiment differs from the first to third embodiments in the following points.

The embodiment uses a pre-knot cartridge 365 like the one shown in FIG. 76, FIG. 86, and FIG. 87. This pre-knot cartridge 365 is comprised of a removable needle 213, suture thread 214, needle-catching-device 212, flexible tubular member 215, and the like. The suture thread 214 is inserted into a hole 366 of the removable needle 213 and has a stopper 272 at its distal end face so as not to come off the removable needle 213. In this embodiment, an end face of a thread is rounded by heat. To fix the thread to the removal needle more firmly, a peripheral portion of the stopper 272 may be coated with an adhesive or the hole 366 may be caulked. Before the end face of the thread is rounded by heat, a knot may be formed at the end face of the thread and thermally molded by a mold which can be divided into two parts and forms a spherical surface. In addition, as shown in FIG. 69, FIG. 76, and FIG. 89, a pre-knot 232 is formed in the suture thread 214 on the surface of the needle-catching-device 212. The pre-knot 232 is preferably tied in the form of a Roeder knot as shown in FIG. 89, which can slide. The suture thread 214 is also slidably inserted into the flexible tubular member 215. The suture thread 214 is formed into a loop 273 on the proximal end side. As shown in FIG. 86 and FIG. 87, the pre-knot 232 is pressed by a cover 274 so as not to come off the needle-catching-device 212 before the use of the

pre-knot cartridge 365.

As shown in FIG. 69, a needle-catching-sheath 211 is comprised of a distal tip 249, a flexible tubular member 247, a flexible rod 248 inserted into the inner
5 hole of the flexible tubular member 247, and the like. A female screw 250 is formed on the distal tip 249. The flexible rod 248 is fixed to the other end of the distal tip 249. The flexible rod 248 prevents the expansion of the flexible tubular member 247 upon
10 application of a force.

In place of the needle-catching-sheath 211, a needle-catching-sheath 527 like the one shown in FIG. 99 may be used. The needle-catching-sheath 527 is comprised of a distal tip 528, a flexible tubular
15 member 529 (made of, for example, a flat coil), a connecting member 530 which connects the flexible tubular member 529 to the flexible tubular member 531, a connecting member 532 connected to a handle 533 on the proximal end side of the flexible tubular member
20 531, a buckling preventing means 536 that partly covers the flexible tubular member 531 and connecting member 532 by thermal contraction, a stylet 534 for preventing the elongation of the flexible tubular member 529 and flexible tubular member 531 having both ends connected
25 to the distal tip 528 and connecting member 532, a flexible tubular body 535 (e.g., a tube made of fluoroplastic) fitted on the outer surface of the

flexible tubular member 529 by thermal contraction, and the like.

Unlike the needle-catching-sheath 211, the needle-catching-sheath 527 has the flexible tubular body 535. Even if, therefore, a suturing operation to be described later (FIG. 90 to FIG. 98) is performed after the pre-knot 232 is placed on the flexible tubular body 535, the thread is not caught between windings forming the flexible tubular member 529. In addition, since the flexible tubular body 535 allows the thread to slide more smoothly than a coil, it facilitates removing the pre-knot 232 from the needle-catching-sheath as shown in FIG. 94 and FIG. 95.

As shown in FIG. 69, a channel member 367 is comprised of a distal pipe 233, a tube 245 fixed to the distal pipe 233, and the like, and fixed to a holding member 223 through a support member 234. Holes 368 and 369 having different diameters are formed in the distal pipe 233. The diameter of the hole 369 is designed to be slightly larger than the outer diameters of the needle-catching-sheath 211 and needle-catching-device 212 and smaller than the outer diameter of the pre-knot 232. The needle-catching-sheath 211 is inserted into the distal pipe 233 through the inner hole of the channel member 367 having almost the same diameter as that of the hole 369. The needle-catching-sheath 211 as a constituent element of the pre-knot cartridge

365 is detachably connected to the distal end of the
needle-catching-sheath 211 with screws. The needle-
catching-device 212 is detachably connected to the
distal tip 249 with screws and loaded into the hole
5 368. The removable needle 213 of the pre-knot
cartridge 365 is detachably fixed to a needle holder
216, as shown in FIG. 69. The suture thread 214 is
placed in a groove 217 formed in the needle holder 216.

As shown in FIG. 173 and FIG. 174, a slit 537 may
10 be formed in the needle holder 216. The formation of
such a slit gives elasticity to the fitting portion
between the needle holder 216 and the removable needle
213, thereby forming a press-fitting structure that
prevents the removable needle 213 from easily coming
15 off the needle holder 216. As shown in FIG. 69 to
FIG. 77 and 80, the needle-catching-device 212 is
comprised of a needle-catching-body 275, inserting
member 276, and spring 277.

As shown in FIG. 78, when the needle-catching-
20 sheath 211 is moved to the left on the drawing surface,
the removable needle 213 is inserted into an
infundibular recess part 278 of the inserting member
276 and spreads the spring 277 (see FIG. 88). When the
needle-catching-sheath 211 is further moved, the spring
25 277 returns to its original shape and comes into
contact with a contact face 370 formed on the removable
needle 213, as shown in FIG. 79. This makes it

possible to lock the removable needle 213 to the needle-catching-device 212, as shown in FIG. 80.

The needle holder 216 has a taper 253 to reduce the resistance produced when it punctures the tissue.

5 As shown in FIG. 74 and FIG. 75, an operating section 255 of the suturing device is arranged on the proximal end side of flexible tubular members 225 and 226 and transmission member 224. The operating section 255 incorporates a ratchet mechanism. When a button
10 261 is pressed as shown in FIG. 74, the ratchet mechanism is released to allow a slider 257 to be freely pushed and pulled. When the button 261 is slid to the right side on the drawing surface, a stopper 267 formed on the button 261 is unlocked from an engage
15 part 268 formed on the slider 257, and an engage part 262 that has been biased by a spring 263 is pressed downward. As a consequence, the engage part 262 engages with a burr member 260 formed in an operating section body 256. The slider 257 can move only to the
20 right. This inhibits first and second active members 218 and 219 from moving in a direction to open.

On the other hand, as shown in FIG. 69, the flexible tubular member 215 of the pre-knot cartridge 365 is pressed into a recess 241 of a holder 240 fixed
25 to the tube 245. In this case, since the flexible tubular member 215 is formed from a flexible resin member such as a silicone member, the suture thread 214

can slide with respect to the flexible tubular member 215 even while the flexible tubular member 215 is pressed in the recess 241.

5 The structures of the needle-catching-device 212, removable needle 213, and needle holder 216 in this embodiment may be changed into those shown in FIG. 81 to FIG. 85.

10 As shown in FIG. 81 and FIG. 88, a needle-catching-device 283 is comprised of a needle-catching-body 279, inserting member 280, spring 281, and the like. As shown in FIG. 81, when the needle-catching-device 283 is moved to the left on the drawing surface, a removable needle 364 is inserted into an infundibular recess part 282 of the inserting member 280 and spreads
15 the spring 281 (see FIG. 88). When the needle-catching-device 283 is further moved, the spring 281 returns to its original shape, as shown in FIG. 83. As a consequence, the spring 281 engages with a recess 371 formed in at least part of the removable needle
20 364. When the needle-catching-device 283 is moved to the right on the drawing surface thereafter as shown in FIG. 84, the spring 281 including the removable needle 364 moves until it comes into contact with a contact face 372 formed on the inserting member 280. As a
25 result, the movement of the spring 281 in a direction to spread is restricted by the wall of an engage part 285 formed on the inserting member 280, and hence the

removable needle 364 can be locked to the needle-catching-device 283.

5 The removable needle 364 has the recess part 371 to reduce the resistance produced when it punctures the tissue. As shown in FIG. 175 and FIG. 176, a slit 538 may be formed in the needle holder 216 without the taper 253 to form a press-fitting structure in which the fitting between the removable needle 364 and the needle holder 216 is not easily released.

10 (Function)
A suturing procedure will be described with reference to FIG. 90 to FIG. 97.

15 (1) A suturing device 210 protected by the insert assisting devices 84 and 95 in the first embodiment, the protect member 100 in the second embodiment, or the protect member 122 in the third embodiment is inserted into the body.

20 (2) As shown in FIG. 90 and FIG. 91, the removable needle 213 and two fixing needles 229 are so pressed against the region to be sutured as to close the first and second active members 218 and 219, and the tissue is punctured with the removable needle 213.

25 (3) As shown in FIG. 92, after puncturing, the needle-catching-sheath 211 is pushed into the removable needle 213, and the needle-catching-device 212 is engaged with the removable needle 213.

(4) As shown in FIG. 93, the

needle-catching-sheath 211 is pulled, and the removable needle 213 is withdrawn from the needle holder 216.

(5) As shown in FIG. 94, the first and second active members 218 and 219 are opened to withdraw the
5 needle holder 216 from the tissue.

(6) As shown in FIG. 95, the needle-catching-sheath 211 is further pulled to remove the pre-knot 232 from the needle-catching-device 212.

(7) As shown in FIG. 96 and FIG. 97, the
10 needle-catching-sheath 211 is further pulled to move the pre-knot 232 to the opening portion of the tissue, and the opening portion is sutured.

(8) As shown in FIG. 98, a redundant portion of the thread is cut by using a thread cutting device 136
15 or the like.

(Effects)

In addition to the advantages of the first and second embodiments described above, according to this embodiment, since there is no need to make a knot
20 outside the body and feed it into the body, the manual operation time can be shortened, and the procedure is further facilitated. In addition, there is no need to indwell any member other than the suture thread in the body.

25 [11th Embodiment]

FIG. 100 to FIG. 111 show the 11th embodiment.

(Arrangement)

The 11th embodiment differs from the 10th embodiment in the following points.

As shown in FIG. 101, the interval between pins
5 303 and 304 of a suturing device 373 of the 11th
embodiment is larger than that between the pins 235 and
236 in the 10th embodiment. In addition, the interval
between the pin 303 and a pin 305, the interval between
the pin 304 and a pin 306, the interval between the pin
10 305 and a pin 307, and the interval between the pin 306
and the pin 307 are larger than those in the 10th
embodiment. As shown in FIG. 108, this arrangement
allows a first actuating member 287 to make a larger
rotational movement than the first active member 218
15 (see FIG. 90) in the 10th embodiment, and also can
increase the puncturing force acting on a removable
needle 213 fixed to a needle holding member 310.

As shown in FIG. 102 and FIG. 106, a second active
member 288 can rotate about the pin 304. A pipe 375 is
20 rotatably fitted on part of the pin 304, and a spring
308 is arranged around them. An arm member 376 of the
spring 308 is in contact with a contact face 378 formed
on the second active member 288. As shown in FIG. 107,
a force charging member 300 is connected, through the
25 pin 306, to a second connecting member 290 which is
connected to a rod 291 to be rotatable about the pin
307. This force charging member 300 can pivot about

the pin 304. The other arm member 377 of the spring 308 is so arranged as to come into contact with a ring member 311 pivotally mounted on a cylinder part 379 of the force charging member 300 formed on the axis of the pin 306. In this case, the ring member 311 is arranged to reduce the resistance of the arm member 377. Obviously, however, this ring member 311 can be omitted. As in the 10th embodiment, two fixing needles 298 are mounted on a U-shaped end portion of the second active member 288. As shown in FIG. 177, these fixing needles 298 may be needles in the form of eagle's claw with its distal end curving inward. When the tissue is punctured with a fixing needle having such a form, the needle does not easily slip off from the tissue. Such a modification of the fixing needle can also be applied to other embodiments.

As shown in FIG. 101, a stopper 309 is fixed to the second active member 288 to prevent the second active member 288 from further rotating clockwise from the state shown in FIG. 101.

Since a pre-knot cartridge 365, a needle-catching-sheath 211, and an operating section 255 in addition to the removable needle 213, which are other constituent members, are the same as those in the 10th embodiment, a description thereof will be omitted. In addition, this embodiment may use the arrangement of the removable needle 364 and needle-catching-device 283 in

described in the 10th embodiment.

(Function)

The operation of the suturing device 373 in a case wherein the tissue to be sutured is punctured
5 will be described with reference FIG. 108 to FIG. 111.

(1) When the rod 291 is pushed to the left on the drawing surface as shown in FIG. 108 by operating the operating section 255 (not shown), the first active member 287 can be opened to the position shown in
10 FIG. 108. At this time, since no external force is applied to the second active member 288 in a direction to open, the second active member 288 is opened by the spring 308 to only the position shown in FIG. 108. When the removable needle 213 is inserted into the
15 tissue at an angle θ where $45 \text{ degrees} < \theta < 110$ degrees (preferably, 90 degrees), the tissue is punctured deep. This makes it possible to reliably suture the tissue.

(2) As shown in FIG. 109, when the second
20 actuating member 219 is moved to the right on the drawing surface, the tissue is punctured with the removable needle 213 and two fixing needles 229. At this time, the counterclockwise force acting on the second active member 288 is equal to the biasing force
25 of the spring 308.

(3) As shown in FIG. 110 and FIG. 111, when the rod 291 is further moved to the right on the surface

drawing, a contact face 312 of the force charging member 300 engages with a contact face 380 of the second active member 288. As a consequence, in addition to the biasing force, the force of the force charging member 300 acts on the second active member 288. This makes it possible to reliably rotate the second active member 288 clockwise. As shown in FIG. 111, to completely close the first active member 287 even when a large portion of the tissue is caught, the position where the contact face 312 engages with the contact face 380 is set in a direction in which the second active member 288 opens. In other words, while no tissue is caught, the second active member 288 is in contact with the first active member 287 with only the force of the spring 308. At this time, the contact face 312 is not in contact with the contact face 380. This makes it possible to match the axis of the removable needle 213 in FIG. 101 with that of the needle-catching-device 212 to a certain extent.

Therefore, the needle-catching-device 212 can easily recover the removable needle 213. Since a suturing procedure is the same as that in the 10th embodiment (see FIG. 90 to FIG. 98), a description thereof will be omitted.

(Effects)

In addition to the effects of the 10th embodiment, the tissue can be punctured deeper, and the removable

needle 213 can be easily recovered.

[12th Embodiment]

FIG. 112 to FIG. 122 show the 12th embodiment.

(Arrangement)

5 The 12th embodiment differs from the 10th
embodiment in the following points.

 As shown in FIG. 113, the interval between pins
329 and 330 of a suturing device 374 of the 12th
embodiment is larger than that between the pins 235 and
10 236 in the 10th embodiment. In addition, the interval
between the pin 329 and a pin 331, the interval between
the pin 330 and a pin 332, the interval between the pin
331 and a pin 333, and the interval between the pin 332
and the pin 333 are also larger than those in the
15 10th embodiment. As in the 11th embodiment, this
arrangement allows a first active member 313 to make
a larger rotational movement, and also can increase the
puncturing force acting on a removable needle 213 fixed
to a needle holding member 336.

20 As shown in FIG. 114 and FIG. 117, a second active
member 314 can rotate about the pin 330. A pipe 381 is
rotatably fitted on part of the pin 330, and a spring
334 is arranged around them. An arm member 382 of the
spring 334 is in contact with a contact face 340 formed
25 on the second active member 314. As shown in FIG. 118,
a force charging member 326 is connected, through the
pin 332, to a second connecting member 316 which is

connected to a rod 317 to be rotatable about the pin 333. A first arm member 325 can pivot about the pin 329. The other arm member 383 of the spring 334 engages with a pin 339 fixed to a holding member 318.

5 In addition, as in the 10th embodiment, two fixing needles 324 are mounted on a U-shaped end portion of the second active member 314.

As shown in FIG. 113 and FIG. 119, a stopper 335 is fixed to the second active member 314 to prevent
10 the second active member 314 from further rotating counterclockwise from the state shown in FIG. 119.

Since a pre-knot cartridge 365 containing the removable needle 213, a needle-catching-sheath 211, and an operating section 255, which are other constituent
15 members, are the same as those in the 10th embodiment, a description thereof will be omitted. In addition, this embodiment may use the arrangement of the removable needle 364 and needle-catching-device 283 in described in the 10th embodiment.

20 (Function)

The operation of the suturing device 374 in a case wherein the tissue to be sutured is punctured will be described with reference to FIG. 119 to FIG. 122.

(1) When the rod 317 is pushed to the left on the
25 drawing surface as shown in FIG. 119 by operating the operating section 255 (not shown), the first active member 313 can be opened to the position shown in

FIG. 119. At this time, although a counterclockwise force is biased against the second active member 314, the member is opened by the spring 335 to only the position shown in FIG. 119. Note, however, that this device is designed to reduce the biasing force of the spring 334 in the state shown in FIG. 119. When the removable needle 213 is inserted into the tissue at an angle θ where $45 \text{ degrees} < \theta < 110 \text{ degrees}$ (preferably, 90 degrees) as in the 11th embodiment, the tissue is punctured deep. This makes it possible to reliably suture the tissue.

(2) As shown in FIG. 120, when the rod 317 is moved to the right on the drawing surface, the tissue is punctured with the removable needle 213 and two fixing needles 229. At this time, since the second active member 314 is biased counterclockwise, the member does not rotate.

(3) As shown in FIG. 121 and FIG. 122, when the rod 317 is further moved to the right on the surface drawing, a contact face 341 of the force charging member 326 engages with a contact face 342 of the second active member 314. As a consequence, the second active member 314 rotates in a clockwise direction. Since a suturing procedure is the same as that in the 10th embodiment (see FIG. 90 to FIG. 98), a description thereof will be omitted.

(Effects)

In addition to the effects of the 10th embodiment, the tissue can be punctured deeper.

[13th Embodiment]

5 FIG. 123 to FIG. 126B show the 13th embodiment.

(Arrangement)

In the 13th embodiment, the arrangement of the 12th embodiment is modified as follows.

10 The spring 334 and pin 339 are removed. A stopper 384 is fixed to a second active member 349. As shown in FIG. 126B, a holding member 353, a first active member 348, and the second active member 349 are partly thinned.

(Function)

15 The operation of a suturing device 385 in a case wherein the tissue to be sutured is punctured will be described with reference FIG. 123 to FIG. 126A.

20 (1) When a rod 352 is pushed to the left on the drawing surface as shown in FIG. 123 by operating an operating section 255 (not shown) as in the 12th embodiment, a needle holder 357 can be opened to the position shown in FIG. 123. At this time, the second active member 349 opens to the position shown in FIG. 123 because a transmission member 355 interferes with a contact face 386 of the second active member 349.

25 (2) As shown in FIG. 124, when the rod 352 is

5 moved to the right on the drawing surface, the tissue is punctured with the removable needle 213 and two fixing needles 363. At this time, as shown in FIG. 124, the second active member 349 is pressed against the tissue and is biased counterclockwise by the resultant reaction force.

10 (3) As shown in FIG. 125 and FIG. 126A, when the rod 352 is further moved to the right on the surface of the drawing, a contact face 387 of the transmission member 355 engages with a contact face 388 of the second active member 349. As a consequence, the second active member 349 rotates clockwise. Since a suturing procedure is the same as that in the 10th embodiment (see FIG. 90 to FIG. 98), a description thereof will be omitted.

15 (Effects)

In addition to the effects of the 10th embodiment, the tissue can be punctured deeper. Furthermore, the suturing device can be thinner than the devices of the 11th and 12th embodiments. This improves the field of view.

20 [14th Embodiment]

FIG. 127 to FIG. 128B show the 14th embodiment.

(Arrangement)

25 In the 14th embodiment, the suturing device of the first embodiment or another embodiment is designed to extend and retract from an endoscope as shown in

FIG. 127.

The tubes 245 and 227 described in the first embodiment and the like are retractably inserted in the inner holes of a tube holding member 343 and tubes 345 and 344. Valves for hermetic sealing are arranged on the proximal end side of the tubes 344 and 345 to allow the tubes 245 and 227 to extend and retract while keeping the airtightness in the tubes 344 and 345. The tube holding member 343 is fixed near the distal end of the endoscope with a fixing member 346. The fixing member 346 may be an adhesive tape, press-fitting scheme, or the like.

In addition, as shown in FIG. 128B, a protect member 347 may be fixed to the tube holding member 343 and inserted into the body without using the insertion assisting tool 84 shown in FIG. 16 or the like.

(Function)

The suturing device is made to extend/retract with respect to the endoscope and approach a region to be sutured by pushing and pulling the proximal end portions of the tubes 245 and 227 with respect to the tubes 344 and 345.

(Effects)

The suturing device can be easily made to approach a region to be sutured.

After the suturing device is made to approach the region, the region can be sutured deeper by pressing

the device against the tissue.

[15th Embodiment]

FIG. 129 to FIG. 143 show the 15th embodiment.
(Arrangement)

5 The 15th embodiment is configured to continuously suture the tissue by using the suturing device exemplified by the fourth to 14th embodiments.

 As shown in FIG. 129, in the 15th embodiment, each of the needle holders 216, 336, and 357 in the fourth
10 to 13th embodiments are modified into a needle holder 396. Likewise, the pre-knot cartridge 365 is modified into a pre-knot cartridge 407, and each of the needle-catching-devices 212 and 283 is modified into a needle-catching-device 390. The pre-knot cartridge
15 407 is comprised of a removable needle 389, thread 391, pre-knot 397, and the like. The removable needle 389 is comprised of a needle 392, slide member 393, spring 399, lock members 394 and 395, and the like. As in the case of the removable needle 213 in the 10th
20 embodiment, the thread 391 is fixed to the needle 392 with a stopper 408 formed on the thread. The slide member 393 and needle 392 are slidably fitted together. The slide member 393 is biased to the left on the drawing surface by the spring 399. The needle 392 is
25 engaged with the needle holder 396 by the lock member 394, 395. In the state shown in FIG. 129, the removable needle 389 does not come off the needle holder 396.

The needle-catching-device 390 is comprised of a tip member 402, inserting member 403, spring 401, release member 404, and the like. Although not shown, the proximal end portion of the tip member 402 is connected
5 to a flexible member like the needle-catching-sheath 211. As shown in FIG. 129, the spring 401 is connected to the release member 404 and can be moved to the right on the drawing surface. An operating section (not shown) is attached to the proximal end portion of the
10 release member 404 to allow the release member 404 to extend and retract.

The pre-knot 397 is wound around the needle-catching-device 390.

(Function)

15 A continuous suturing procedure will be described below.

(1) As shown in FIG. 129, the removable needle 389 is inserted into the tissue.

(2) When the needle-catching-device 390 is moved
20 to the left on the drawing surface as shown in FIG. 130, the spring 401 spreads as shown in FIG. 130 and engages with a recess 400 of the slide member 383 as shown in FIG. 131.

(3) When the needle-catching-device 390 is moved
25 to the right on the drawing surface as shown in FIG. 132, the spring 401 moves to the left on the drawing surface. As a result, an engage part 405

restricts the spreading of the spring 401.

(4) When the needle-catching-device 390 is moved to the right on the drawing surface as shown in FIG. 133, the spring 399 that has biased the slide member 393 to the left on the drawing surface, is
5 compressed to move the slide member 393 to the right on the surface drawing. At this time, the lock members 394 and 395 are released from the restriction in the vertical direction on the drawing surface, and can move
10 as shown in FIG. 133. In this manner, as shown in FIG. 134, the removable needle 389 is removed from the needle holder 396.

(5) The needle holder 396 is pulled out from the tissue as shown in FIG. 135, and is then returned to
15 the illustrated position shown in FIG. 136.

(6) When the needle-catching-device 390 is moved to the left on the drawing surface as shown in FIG. 137, the lock members 394 and 395 move on the engage member 398. At this time, the lock members 394
20 and 395 partly enter recesses 406 and 409 formed in the slide member 393, and hence can move on the engage member 398. In this manner, as shown in FIG. 138, the removable needle 389 can be mounted in the needle holder 396 again.

(7) As shown in FIG. 139, the release member 404
25 is moved to the right on the drawing surface by operating the operating section (not shown) to return

the spring 401 to the illustrated position in FIG. 139. When the needle-catching-device 390 is moved to the right on the drawing surface while this state is kept, the spring 401 spreads and comes off the slide member 393, as shown in FIG. 140 and FIG. 141.

(8) The tissue is continuously sutured by repeating the above operation. When the tissue is completely sutured, a continuous suturing operation like that shown in FIG. 142 and FIG. 143 can be done by making a knot like the one shown in FIG. 94 to FIG. 98. (Effects)

In addition to the effects of the fourth to 14th embodiments, the tissue can be continuously sutured. [16th Embodiment]

FIG. 144 to FIG. 163 show the 16th embodiment. (Arrangement)

The 16th embodiment differs from the 11th embodiment in the following points.

Since the length of a spring 432 is decreased as compared with that in the 11th embodiment shown in FIG. 102, a projection member 466 formed on the distal end of a holding member 292, which interferes with the field of view of an endoscope, is omitted. This improves the field of view in a suturing operation (see FIG. 145).

In this embodiment, a suturing operation is performed by using an end loop cartridge 440 shown in

FIG. 146 and FIG. 158 in place of the pre-knot cartridge 365 in the 11th embodiment. The end loop cartridge 440 is comprised of a removable needle 441, suture thread 442, needle lock mechanism 475, casing member 446, releasing member 447, elastic member 448, rigid member 449, and the like.

Referring to FIG. 146 and FIG. 158, the suture thread 442 fixed to the removable needle 441 is pressed into the elastic member 448 arranged in the casing member 446 through holes 450 and 457 formed in the needle lock mechanism 475. This thread further extends through a hole 476 formed in the releasing member 447 to form a loop 451 on the proximal end side.

To increase the sliding resistance between the elastic member 448 and the suture thread 442, the rigid member 449 is tightly attached to the elastic member 448 by swaging, caulking, or the like. A lock member 454 formed on the releasing member 447 engages with a hole 456 formed in the casing member 446 to prevent the releasing member 447 from coming off the casing member 446. The removable needle 441 is detachably forced into a needle holding member 434. In this case, the removable needle 441 and needle holding member 434 may be designed such that a removable needle 489 having a groove 490 is fitted in the needle holding member 434 having an elastically deformable stopper 492 as shown in FIG. 165 and FIG. 166 to prevent the removable

needle 489 from easily coming off a needle holding member 491. Alternatively, as shown in FIG. 175 and FIG. 176, a slit like the one shown in FIG. 175 and FIG. 176 may be formed in the needle holder to prevent
5 the removable needle 441 from easily coming off the holder.

The casing member 446 is fitted in a distal pipe 425.

As shown in FIG. 147 and FIG. 159, an engage tube
10 465 comprised of two engage members 458, a pipe 459 which fixes the proximal end portions of the engage members, a tube 460 coupled to the pipe 459, and the like is designed to allow a hook device 461 to freely extend and retract. The hook device 461 is comprised
15 of a flexible coil 462, a hook 463, a transmission member 464 fixed to the hook 463, and an operating section (not shown). The hook 463 can be made to extend and retract by operating the operating section. A seal structure made of an O-ring and the like is
20 formed on the proximal end side of the engage tube 465 to ensure airtightness between itself and the hook device 461.

As shown in FIG. 144, a holding member 416 has a cylinder part 467 and is retractably arranged in
25 an outer sheath 468. In addition, as shown in FIG. 144 and FIG. 160, the outer sheath 468 is comprised of a guide pipe 436, guide tube 437, port 471, seal member

472, and the like. With this arrangement, a tube 420 of a suturing device 410 can keep airtightness inside the outer sheath 468. An inner sheath 479 shown in FIG. 144 and FIG. 161 is comprised of a tube 439 and
5 port 474 coupled to the distal pipe 425, and a seal member 478, and the like, and is inserted into an outer sheath 480 having a larger inner diameter. In this case, the outer sheath 480 is comprised of a guide tube 438, port 473, seal member 477, and the like. With
10 this structure, airtightness in the outer sheath 480 is maintained by the seal member 477. The engage tube 465 in which the hook device 461 shown in FIG. 147 is inserted is inserted into the inner sheath 479 through the seal member 478. At this time, the airtightness
15 between the tube 460 and the seal member 478 is also maintained.

Referring to FIG. 144, the outer sheath 468 and inner sheath 479 are respectively formed from the flexible tubular members 437 and 439. As shown in
20 FIG. 163, however, portions of these members which do not reach the curved portion of the distal end portion of the endoscope when the suturing device 410 is mounted in the endoscope may be modified into hard tubes 481 and 482 (e.g., tubes in which thin wires are
25 embedded in a lattice form) which hardly extend and contract. This makes it possible to apply a large force to members inserted into the outer sheath 468 and

inner sheath 479 without interfering with the bending operation of the endoscope.

5 The engage tube 465 in which the hook device 461 is inserted as shown in FIG. 147 extends through the seal member 478 shown in FIG. 161 and comes off the distal pipe shown in FIG. 144. By operating the operating section (not shown) of the hook device 461 coming off the distal pipe, the loop 451 of the end loop cartridge 440 is hung on the hook 463 and the hook 10 463 is pulled in, as shown in FIG. 147. As shown in FIG. 147, FIG. 158, and FIG. 157, the lock member 458 of the engage tube 465 is engaged with a hole 455 of the end loop cartridge 440, and is then loaded into the distal pipe shown in FIG. 144. FIG. 164 shows the 15 loaded state.

The structure in which the removable needle 441 is locked to the needle lock mechanism 475 is the same as that shown in FIG. 81 to FIG. 85.

(Function)

20 A suturing procedure will be described below with reference to FIG. 147 to FIG. 157. For the sake of easy understanding of operation, an illustration of the suturing device 410 is omitted from FIG. 147 to FIG. 157. In reality, therefore, a suturing operation 25 is performed while the end loop cartridge 440 is loaded as shown in FIG. 164.

(1) The operating section of the suturing device

410 (not shown) is operated to puncture the tissue with the removable needle 441 as shown in FIG. 147.

(2) As shown in FIG. 148, the hook device 461 and engage tube 465 are pushed into the end loop
5 cartridge 440 to make the removable needle 441 engage with the needle lock mechanism 475 of the end loop cartridge 440.

(3) As shown in FIG. 149, when the hook device 461 and engage tube 465 are moved to the right on the
10 drawing surface, the removable needle 441 is unlocked from the needle holding member 434. At this time, since the lock member 458 is engaged with a needle-catching-body 445 of the end loop cartridge 440, the removable needle 441 can be reliably unlocked from the
15 needle holding member 434.

(4) As shown in FIG. 150, when the hook device 461 is pushed to the left side on the drawing surface, the releasing member 447 is pushed into the casing member 446, and an inclined portion 453 is engaged
20 with the hole 455. At this time, since the lock member 458 moves on the inclined portion 453, the member is unlocked from the hole 455 (see FIG. 151). In addition, since the casing member 446 elastically deforms, the releasing member 447 can engage with the
25 hole 455.

(5) As shown in FIG. 152, the needle holding member 434 is pulled off from the tissue.

(6) As shown in FIG. 153 and FIG. 154, the hook 463 is pulled to fasten the suture thread 442. At this time, the sliding friction between the suture thread 442 and the elastic member 448 prevents the sutured region from loosening.

(7) As shown in FIG. 155 and FIG. 156, the hook 463 is pulled out from the coil 462, and the loop 451 is unfastened from the hook 463.

(8) As shown in FIG. 157, a redundant portion of the suture thread 442 is cut by using a thread cutting forceps 469. In this case, as shown in FIG. 162, the thread cutting forceps 469 is designed to cut the thread by opening/closing scissors members 483 and 484 having sharp cutting blades. In addition, the thread cutting forceps 469 has recess parts 485 and 486 to prevent the thread from escaping from the blades when it is cut. Furthermore, a rotatable sheath 487 allows the thread cutting forceps 469 to rotate about the axis, and hence the direction of the scissors members 483 and 484 can be freely changed. Since the suture thread 442 is exposed in a space 488 as shown in FIG. 157, when the operator wants to remove the end loop cartridge 440 after a suturing operation, he/she can easily remove the end loop cartridge 440 from the tissue by cutting this portion of the suture thread 442.

(Effects)

In addition to the effects of the 10th embodiment, the end loop cartridge 440 can be easily removed from the sutured region. In addition, this device allows an easy approach to a region to be sutured. Furthermore, after an approach to the tissue, the tissue can be sutured deep by pressing the suturing device against the tissue.

[17th Embodiment]

FIG. 169 to FIG. 171 show the 17th embodiment.

(Arrangement)

The 17th embodiment differs from the 16th embodiment in the following points.

As shown in FIG. 169 to FIG. 171, a third actuating member 494 is pivotally coupled to a first actuating member 501 and third connecting member 502 by using pins 511 and 510, respectively. The first actuating member 501 is pivotally coupled to a holding member 499 with a pin 504 serving as a holding shaft, and is also coupled to a first connecting member 496 with a pin 507. The third connecting member 502 is pivotally coupled to the holding member 499 with a pin 509. A second actuating member 495 is pivotally coupled to the holding member 499 with a pin 505 serving as a holding shaft, and is also pivotally coupled to a second connecting member 497 with a pin 508. The first and second connecting members 496 and

497 are pivotally coupled to a push rod 498 with a pin 506. As shown in FIG. 169 and FIG. 170, the first and second actuating members 501 and 495 can be opened/closed by pushing and pulling the rod 498.

5 With this operation, the third actuating member 494 is moved by the first and third actuating member 501 and 502. Other arrangements are the same as those in the 16th embodiment, and hence a description thereof will be omitted.

10 (Function)

A suturing operation is performed in the same manner as in the sixth embodiment shown in FIG. 147 to FIG. 157. In FIG. 169 and FIG. 170, the end loop cartridge 440, the distal pipe, and the like are
15 omitted.

(Effects)

In addition to the 16th embodiment, the locus of the distal end of a removable needle 441 can be made a one different from a circular locus around the pin 504.
20 This makes it possible to puncture the tissue deeper.

The stroke of the push rod 498 which is required to open/close the third and second actuating members 494 and 495 can be reduced.

[18th Embodiment]

25 FIG. 172 shows the 18th embodiment.

(Arrangement)

The 18th embodiment differs from the 16th

embodiment in the following points.

As shown in FIG. 172, this embodiment has first and second catching members 519 and 520 pivotable about pins 522 and 523. Needle-like members are formed on the distal ends of the first and second catching members 519 and 520 to prevent them from sliding on the tissue when they catch it. In addition, the first and second catching members 519 and 520 can operate independently of the opening/closing operation of first and second actuating members 517 and 518 owing to a link structure (not shown). Other arrangements are the same as those in the 16th embodiment, and hence a description thereof will be omitted.

(Function)

A suturing operation is performed in the same manner as in the 16th embodiment shown in FIG. 147 to FIG. 157. Note, however, that the tissue is caught by using the first and second catching members 519 and 520 before the tissue is punctured with a removable needle 441, and the tissue is punctured with the removable needle 441 after the tissue is pulled up.

(Effects)

In addition to the effects of the 16th embodiment, since the tissue can be punctured with the removable needle 441 while the tissue is pulled up by the first and second catching members 519 and 502, the tissue can be punctured deeper.

[19th Embodiment]

FIG. 178 and FIG. 179 show the 19th embodiment.
(Arrangement)

The 19th embodiment differs from the 16th
5 embodiment in the following points.

As shown in FIG. 178 and FIG. 179, the end loop
cartridge 440 is modified into an end loop cartridge
539, and the engage tube 465 is modified into an engage
tube 543.

10 The end loop cartridge 539 is comprised of
a removable needle 441 similar to the one in the
16th embodiment, a suture thread 442, a needle lock
mechanism 475, an elastic member 448, a rigid member
449, a casing member 540, and the like. The engage
15 tube 543 is comprised of two lock members 545, a pipe
549 that fixes the proximal end portions of these lock
members, a tube 550 coupled to the pipe 549, and the
like, and is designed to allow a hook device 461 to be
retractably arranged inside.

20 As shown in FIG. 178, after a loop 451 of the end
loop cartridge is hung on a hook 463 of the hook device
and the loop 451 and suture thread 442 are partly
pulled into the hook device 461, two lock members 545
of the engage tube 465 are positioned to holes 546
25 formed in the casing member 540. Thereafter, as shown
in FIG. 179, the hook device 461 is moved to the left
on the drawing surface to push the lock members 545

upward in the vertical direction on the drawing surface so as to make it engage with the hole 546. With this operation, the engage tube 543 and end loop cartridge 539 can integrally engage with each other. In
5 addition, the lock members 545 have elastic arms 559.
(Function)

A suturing procedure is almost the same as that in the 16th embodiment shown in FIG. 147 to FIG. 157 except for the following point.

10 The operation of disengaging the end loop cartridge 440 from the engage tube 465, which is shown in FIG. 149 and FIG. 150, is modified into the operation shown in FIG. 178 and FIG. 179. In this case, the lock members 545 is unlocked from the hook
15 device 461 by moving the hook device 461 to the right on the drawing surface, and the lock members 545 comes off the hole 546 owing to the elasticity properties of the arms 559.

Other operations are the same as those in the 16th
20 embodiment, and hence a description thereof will be omitted.
(Effect)

In addition to the effects of the 16th embodiment, the attachment/detachment of the end loop cartridge 539
25 and engage tube 543 is facilitated.
[20th Embodiment]

FIG. 180 and FIG. 181 show the 20th embodiment.

As shown in FIG. 180 and FIG. 181, the end loop cartridge 440 is modified into an end loop cartridge 539, the engage tube 465 is modified into an engage tube 551, and the distal pipe 425 is modified into
5 a distal pipe 552.

The end loop cartridge 539 is comprised of a removable needle 441 similar to the one in the 16th embodiment, a suture thread 442, a needle lock mechanism 475, an elastic member 448, a rigid member
10 449, a casing member 540, and the like. The engage tube 551 is comprised of two lock members 553, a pipe 554 which fixes the proximal end portions of these lock members, a tube 555 coupled to the pipe 554, and the like, and is designed to allow a hook device 461 to be
15 retractably arranged inside.

As shown in FIG. 180, after a loop 451 of the end loop cartridge is hung on a hook 463 of the hook device and the loop 451 and suture thread 442 are partly pulled into the hook device 461, two lock members 553
20 of the engage tube 551 are positioned to holes 546 formed in the casing member 540. Thereafter, as shown in FIG. 181, the engage tube 551 and hook device 461 are moved to the left on the drawing surface to house the end loop cartridge 539, engage tube 551, and hook
25 device 461 in the distal pipe 552. At this time, when the outer surfaces of the lock members 553 come into contact with the inner surface of hole 556 formed

in the distal pipe 552, arms 558 elastically deform. As a result, the lock members 553 engage with the holes 546. With this operation, the engage tube 551 and end loop cartridge 539 integrally engage with each other.

A hole 557 larger in diameter than the hole 556 is formed in the distal pipe 552. In this case, since the distal end portion of the end loop cartridge 539 partly becomes large, the large-diameter hole 557 is formed.

Obviously, however, if the maximum outer diameter of the end loop cartridge 539 is made smaller than the diameter of the hole 556, such a large-diameter hole 557 need not be formed.

(Function)

A suturing procedure is almost the same as that in the 16th embodiment shown in FIG. 147 to FIG. 157 except for the following point.

The operation of disengaging the end loop cartridge 440 from the engage tube 466 shown in FIG. 149 and FIG. 150 is modified into the operation of disengaging the distal pipe 552 from the hole 556 shown in FIG. 180 and FIG. 181. In this case, the engage tube 551 and hook device 461 are moved to the left on the drawing surface.

Other operations are the same as those in the 16th embodiment, and hence a description thereof will be omitted.

(Effects)

In addition to the effects of the 16th embodiment, the attachment/detachment of the end loop cartridge 539 and engage tube 543 is facilitated.

5 [Twenty-first Embodiment]

FIG. 182A to FIG. 190 each show the twenty-first embodiment of the present invention.

(Arrangement)

10 The present embodiment is featured by a configuration of a new end loop cartridge, and is different from the sixteenth embodiment in the following points.

As shown in FIG. 182A, a suturing device 3 according to the embodiment comprises: an engagingly lock member 458; a circular member 681 connected to the lock member; an end loop cartridge 440; and a hook device 463. FIG. 182A shows a state before the end loop cartridge 440 is assembled with the suturing device 3 and shows a state in which an end loop 451 is hooked on the hook 463. The suturing device is shown by partially omitting it.

20 The engagingly lock member 458 may be placed in parallel as shown in FIG. 182B without being limited to an opened state (FIG. 182A). The engagingly lock member 458 can be connected to a circular member 681 via a screw portion 687, as shown in FIG. 182C.

25 As shown in FIG. 183, the end loop cartridge 440 is moved by an operating section (not shown) via the

circular member 681 from a state in which the end scope cartridge 440 is assembled with the suturing device 3 and is housed in a guide member 462 of the suturing device 3, whereby the end loop cartridge 440 can be
5 engaged with a removable needle 441, as shown in FIG. 184.

As shown in FIG. 185 and FIG. 186, the end loop cartridge 440 is formed in a structure similar to that of the sixteenth embodiment, although it is different
10 in shape. As shown in FIG. 187, the end loop cartridge 440 has an external cylinder shape and has a groove portion 600 at the outer periphery thereof. It is preferable that the end loop cartridge 440 be formed of, for example, polyphenyl sulfone, polyphthal amide,
15 polyether ether ketone, a titanium alloy, or pure titanium etc.

The circular member 681 which can be moved by an operating section (not shown) is connected to the engagingly lock portion 458. The engagingly lock
20 portion can be retracted to the inside of the guide member 462 by the operating section and the circular member 681. This engagingly lock member 458 is closed in contact with the guide member 462, and is established in a state engaged with the groove portion
25 600 of the end loop cartridge 440. In this manner, the engagingly lock member 458 can hold the end loop cartridge 440 reliably. A C (chamfered) face 672

(refer to FIG. 182A) is provided at the engagingly lock member 458. It is preferable that the engagingly lock member 458 be formed of an elastic material such as, for example, SUS402J2 (Japanese Industrial Standard).

5 As shown in FIG. 183, a curved portion 676 is provided at a second active member 412 of the suturing device 3, and an inclined portion 677 is provided at the guide member 462.

(Function)

10 Suturing can be carried out as follows.

The engagingly lock member 458 connected to the circular member 681 which can be moved by the operating section at the outside of a body is retracted in advance to the inside of the guide member 462.

15 The operating section (not shown) of the suturing device 3 is operated, whereby the movable needle 441 is punctured into a tissue as shown in FIG. 188A. Then, in a state in which the removable needle 441 is inserted into the tissue, the end loop cartridge 440 is
20 moved in the left direction on the drawing surface, whereby the cartridge is engaged with the removable needle 441 as shown in FIG. 188B.

 Thereafter, from the state shown in FIG. 188B, the end loop cartridge 440 is moved in the right direction
25 on the drawing surface, whereby the removable needle 441 is removed from a needle holding member 434 (of a curved needle) as shown in FIG. 188C, and the removable

needle 441 is recovered by the end loop cartridge 440. At this time, the engagingly lock member 458 is in contact with the guide member 462, does not expand, and is established in a state engaged with the groove
5 portion 660 of the end loop cartridge 440. The engagingly lock member 458 is continued to reliably hold the end loop cartridge.

(Effects)

In addition to the effects of the sixteenth
10 embodiment, the end loop cartridge 440 can be reliably held. In the case of the sixteenth embodiment, since a relative position relationship is displaced in the case where the coil 462 and the hook device 461 are contracted by a stress, there has been a case in which
15 the end loop cartridge is unintentionally removed as shown in FIG. 150. However, in the present embodiment, such a case does not occur.

An outer appearance of the end loop cartridge 440 is formed in a cylindrical shape, the groove portion
20 600 is formed instead of the hole 455 according to the sixteenth embodiment, whereby the end loop cartridge can be mounted in an arbitrary direction with no orientation of mounting.

The engagingly lock member 458 and the circular
25 member 681 are connected to each other via the screw portion 687, whereby both of them can be separated from each other as required. For example, these members are

dissembled by separating them from each other during wash, and washing properties can be improved.

When the suturing device 3 is inserted into the body by the curved portion 676 of the second active member 412 and the inclined portion 677 of the guide member 462, a shape hardly scratched with a tissue can be obtained.

When the end loop cartridge 440 is made of a material such as polyphenyl sulfone, polyphthal amide, or polyetheretherketone, the cartridge is unlikely to be deformed in the body because of its excellent chemical resistance and acid resistance. Further, the cartridge can be assembled by using ultrasonic deposition or laser deposition because of its excellent deposition properties. In addition, pure titanium or a titanium alloy is superior in bio-compatibility. Next, the operation section (not shown) is operated, pulling the needle holding member from the tissue as shown in FIG. 118D. Thereafter, the suture thread 442 is pulled until the hook 463 is moved to the left in the drawing.

The C face 672 is provided at the engagingly lock member 458, whereby an access to the groove portion 600 is provided smoothly. The end loop cartridge 440 can be removed merely by pushing it with the hook 463 in the left direction on the drawing surface as shown in FIG. 190.

The end loop cartridge 440 is moved away from the

lock member 458 as is illustrated in FIG. 188G.

[Twenty-second Embodiment]

FIG. 191 shows the twenty-second embodiment.

FIG. 191 shows a state in which an end loop
5 cartridge 440 is assembled with a suturing device 3,
and is housed in a guide member 462 of the suturing
device 3. This embodiment is different from the
twenty-first embodiment only in the following points.

In the twenty-first embodiment, the hook device
10 461 is configured of a coil 601 and an expansion proof
tube 602 covering the coil. In the twenty-second
embodiment, an expansion proof wire 602a is used
instead of the expansion proof tube 602.

(Function)

15 The function of this embodiment is same as that of
the twenty-first embodiment.

(Effect)

In the twenty-second embodiment, washing
properties are more excellent because no expansion
20 proof tube 602 covering the coil 601 according to the
twenty-first embodiment is provided.

[Twenty-third Embodiment]

FIG. 192A to FIG. 195 each show the twenty-third
embodiment. The present embodiment is different from
25 the sixteenth embodiment in the following points.

(Arrangement)

In the present embodiment, there are provided a

flexible coil 507, a tube 460, an engagement device 503 provided at a distal end of the tube 460, a hook 463, and an end loop cartridge 440.

FIG. 192A shows a state before the end loop
5 cartridge 440 is assembled with a suturing device 3 and a state in which an end loop 451 is hooked on the hook 463. FIG. 192B shows an outer appearance of the end loop cartridge 440. As shown in the figure, an elastic protrusion 504 and a protrusion portion 505 are added
10 as compared with the twenty-first embodiment.

FIG. 193 shows a state in which the end loop cartridge 440 is housed to be mounted on a guide member 462. FIG. 194 is a sectional view of the state shown in FIG. 193. The end loop cartridge 440 is depicted by
15 omitting the inside thereof. FIG. 195 shows a state in which the protrusion 505 of the end loop cartridge 440 has been removed from the engagement device 503.

A groove portion 506 with which the protrusion 505 can be engaged is provided at the engagement device 503
20 provided at the distal end of the tube 460.

(Function)

When the end loop cartridge is mounted, the end loop 451 is hooked on the hook 463, the hook 463 is moved in the right direction on the drawing surface by
25 an operating portion (not shown), and the end loop 451 is retracted. Next, the protrusion portion 505 of the end loop cartridge 440 is housed to be mounted in

accordance with the groove portion 506 of the engagement device 503.

Although not shown, when the end loop cartridge 440 recovers the removable needle 441, the tube 460 is moved in the left direction on the drawing surface by the operating section (not shown), and the end loop cartridge 440 is moved, thereby recovering the needle.

When the end loop cartridge 440 is removed from the engagement device 503, if a force is applied to the coil 507 in the left direction on the drawing surface by the operating section (not shown), the protrusion 505 is broken (removed), whereby the end loop cartridge 440 is removed from the engagement device 503 in the left direction.

(Effects)

As has been described above in association with the twenty-first embodiment, there has been a case in which the end loop cartridge 440 is removed unintentionally in accordance with the sixth embodiment. However, in the case of the present embodiment, in a state in which the end loop cartridge 440 has been mounted, the protrusion portion 505 is not moved upwardly on the drawing and is not removed unintentionally from the engagement device 503 because of the effect of the elastic portion 504.

[Twenty-fourth Embodiment]

FIG. 196 to FIG. 199 each show the twenty-fourth

embodiment. The present embodiment is different from the sixteenth embodiment in the following points.

(Arrangement)

5 A plurality of windows 612 are opened at an engagement device 503. A hook shaped portion 611 is provided at an end loop cartridge 440. Thread lock means 609 for engagingly locking a suture thread 442 is fixed to the end loop cartridge 440.

(Function)

10 When the end loop cartridge 440 is mounted on the engagement device 503, an end loop 451 is hooked on a hook 463. The hook 463 is moved in the right direction on the drawing surface by an operating section (not shown), and the end loop 451 is retracted. Next, when
15 the end loop cartridge 440 is pushed into the engagement device 503, the hook shaped portion 611 of the end loop cartridge is deformed as shown in FIG. 199, and is mounted as shown in FIG. 196.

20 When the end loop cartridge 440 is removed from the engagement device 503, a flexible coil 607 is moved in the right direction on the drawing surface, whereby the hook shaped portion 611 of the end loop cartridge 440 is deformed as shown in FIG. 199, and is removed.

(Effects)

25 As has been described above in association with the twenty-first embodiment, there has been a case in which the end loop cartridge 440 is removed

unintentionally in the sixteenth embodiment. However,
in the case of the present embodiment, in a state in
which the end loop cartridge has been mounted, the
cartridge is not removed unintentionally from the
engagement member 503 because of the effect of the hook
shaped portion 611.

[Twenty-fifth Embodiment]

FIG. 200 and FIG. 201 each show the twenty-fifth
embodiment.

(Arrangement)

As is evident from a comparison with the hook 463
for use in the sixteenth and twenty-first embodiments
shown in FIG. 200, a slit portion 615 is provided at a
hook 463 according to the present embodiment shown in
FIG. 201.

(Function)

The present embodiment is different from the
sixteenth and twenty-first embodiments in the following
points.

A hook in the shape shown in FIG. 200 serves to
retract the end loop 451 shown in the sixteenth and
twenty-first embodiments in the right direction on the
drawing surface. In FIG. 201, the shape of the hook is
different, and a knot 614 formed in a thread instead of
an end loop is hooked on the slit portion 615 whose
width is smaller than that of the knot, and is moved in
the right direction on the drawing surface, whereby an

attempt is made to achieve the similar effect.

(Effect)

The knot 516 can be produced easily than the end loop 451.

5 [Twenty-sixth Embodiment]

FIG. 202 to FIG. 208 each show the twenty-sixth embodiment.

In FIG. 16 according to the first embodiment, an insert assisting device 84 uses two valves 86 and 87 as
10 means for preventing air leakage. In the present embodiment, the following air tight valve 616 is used.
(Arrangement)

FIG. 202 shows a state in which a suturing device 3 and an endoscope 12 are combined with each other.
15 The suturing device 3 and the endoscope 12 are fixed to each other by using a scope holder 628 and a fixing member 70. FIG. 203 shows a state in which the suturing device 3 and endoscope 12 shown in FIG. 202 are inserted into the insert assisting device 84, and
20 the suturing device 3 is present inside of the insert assisting device 84. FIG. 204 shows a state in which the suturing device 3 is exposed to the outside of the insert assisting device 84 from the state shown in FIG. 203.

25 FIG. 205 shows a state in which the endoscope 12 is passed into the air tight valve 616. FIG. 206 shows an embodiment in which the endoscope 12 is passed

through the air tight valve 616, and further, a metal
or resin based band 618 is wound in order to enhance
air tightness. FIG. 207 shows a state before the band
618 is mounted when it is seen in the direction of an
5 arrow A-A of FIG. 206. FIG. 208 shows a state in which
the band 618 has been mounted when it is seen in the
direction of the arrow A-A of FIG. 206.

The air tight valve 616 according to the present
embodiment is made of a material such as a silicon
10 rubber, a natural rubber, or an isopropylene rubber,
and is fixed to tubes 37, 73 by using an adhesive
material. Then, this valve is used through the
endoscope 12 as shown in FIG. 205. As shown in
FIG. 206 and FIG. 208, in order to ensure fixation
15 between the air tight valve 616 and the endoscope 12,
they can be reinforced by wounding the band 618.
(Function)

As shown in FIG. 205, when the suturing device 3
and the endoscope 12 are fixed to each other, the
20 endoscope 12 is passed through the air tight valve 616.
Further, in the case where the fixation between the air
tight valve 616 and the endoscope 12 is ensured, the
band 618 is wound around the air tight valve 616,
and the fixation is achieved by hooking an U-shaped
25 portion 629.

In any case, as shown in FIG. 203 and FIG. 204,
the air tight valve 616 enters the insert assisting

device before the suturing device 3 is exposed from a distal end 617 of the insert assisting device 84. In addition, when the suturing device reaches a wound portion, the air tight valve 616 is positioned in the insert assisting device.

It is desirable that a full length of the insert assisting device 84 be 500 mm or less, and it is ideal that the full length be 200 mm or less.

(Effect)

While the suturing device 3 is exposed to the outside from the distal end 617 of the insert assisting device 84, the air tightness in a body can be maintained.

[Twenty-seventh Embodiment]

FIG. 209 to FIG. 213 each show the twenty-seventh embodiment. The present embodiment is featured by the operating section for use in the sixteenth and twenty-first embodiments.

(Arrangement)

As shown in FIG. 209 to FIG. 211, sliders 619 and 620 and a knob 621 can be manually moved. A grip 625 serves as a portion at which an operator grips by hand. Further, wash ports 622 to 624 are provided in order to wash the inside of the tube.

When a lock button 626 is operated, the slider 619 is moved only in the left direction on the drawing surface by, for example, a ratchet mechanism (refer to

FIG. 74) described in the tenth embodiment.

As shown in FIG. 211, a guide rod 634 is present inside of a guide pipe 635, and can move relatively. In addition, a rotary knob 630 is fixed to the outside
5 of the guide pipe 635 via a fixing member 636. As shown in FIG. 212 and FIG. 213, the rotary knob 630 has: a groove portion 633 extending at the outer periphery portion along the peripheral direction and axial direction; and a groove portion extending the
10 axial direction, i.e., a straight line portion 638. The groove portion 633 according to the present embodiment is formed symmetrically with respect to a flat plane passing through an axle of the straight line portion 638 and rotary knob 630. A spring 637 is
15 interposed between the rotary knob 630 and the fixing member 636.

(Function)

When the slider 619 is moved in a horizontal direction with respect to the drawing surface, a first
20 active member 411 and a second active member 412 move via a transmission member 417 shown in FIG. 183. When the slider 620 is moved in a horizontal direction with respect to the drawing surface, a hook 463 moves via a transmission member 464. The knob 621 is connected to
25 a coil 601 shown in FIG. 183. When the knob 621 is moved in a horizontal direction with respect to the drawing surface, the coil 601 moves.

Furthermore, FIG. 209 and FIG. 210 each show an embodiment in which the sliders 619 and 620 and the knob 621 which are operating sections are integrated so as to be gripped by a single hand. These sliders 619
5 and 629, knob 621, and lock button 626 are differently colored, respectively.

As shown in FIG. 189 and FIG. 190 according to the twenty-first embodiment, when an end loop cartridge 440 is moved in the left to right direction on the drawing
10 surface, a removable needle 441 slips off from a needle holding member 434 (of a curved needle). As shown in FIG. 211, a guide pin 632 fixed to a connecting plate 631 is engaged with a groove portion 633 (FIG. 212) of the rotary knob 630. By rotating the rotary knob 633,
15 the knob 621 is moved via the connecting plate 631 and the guide rod 634, and a series of reciprocal movement can be carried out.

By rotating the rotary knob 630 and moving the end loop cartridge 440 in the left direction on the drawing
20 surface, when no more movement can be made while in abutment with the needle holding member 434 (FIG. 183), the rotary knob 630 contracts the spring 637 due to its resistive force, and moves in the left direction on the drawing surface, thereby making it possible to relief
25 the stress.

Moreover, when the knob 621 is operated by moving it without using the rotary knob, an angle of the

rotary knob 621 may be set so as to disposed the guide pin 622 at a position of the groove straight line portion 638.

(Effects)

5 The slider 619 and 620 and the knob 621 which are operating sections can be gripped by a single hand all together. In addition, by coloring them differently, a mistake during operation can be prevented, or alternatively, an instruction can be easily supplied.

10 Conventionally, in the case of a method operated by the knob 621, the removable needle 441 has been checked by touch as to whether or not a needle lock mechanism of the end loop cartridge 440 has been reliably actuated. However, in the present embodiment,
15 when the removable needle 441 is removed from the needle holding member 434, the needle can be reliably removed merely by rotating the rotary handle 630.

[Twenty-eighth Embodiment]

20 FIG. 214 to FIG. 216 each show the twenty-eighth embodiment.

(Arrangement)

25 FIG. 214 represents an operating section 641 of the twenty-eighth embodiment. FIG. 215A and FIG. 236B each shows the scope holder 628 shown in FIG. 202 in detail. FIG. 216 shows a state in which a guide rail 639 of the operating section 641 and a guide groove 640 of the scope holder 628 are engaged with each other.

The guide rail 639 is provided at the operating section 641. The guide groove 640 and wash ports 642 and 643 for washing the inside of the tube are provided at the scope holder 628.

5 (Function)

When the guide rail 639 of the operating section 641 and the guide groove 640 of the scope holder 628 are engaged with each other, the operating section 641 and the scope holder 628 can be integrated with each
10 other in the state shown in FIG. 216.

The inside of the tube can be washed by using the wash ports 642 and 643 provided at the scope holder 628. Protection hoods 644, 645 cover the tubes 73, 37.
(Effects)

15 The operating section 641 and the scope holder 628 are integrated with each other, whereby the operating section 641 can be placed anywhere when the end cartridge 440 shown in the twenty-first embodiment or the like is mounted. The protection hoods 644, 645
20 prevent breakage in the case where an excessive force has been applied to the tubes 73, 37.

[Twenty-ninth Embodiment]

FIG. 217 to FIG. 223C each show the twenty-ninth embodiment.

25 As shown in FIG. 217 and FIG. 218, a scope holder 628 comprises: a protrusive and recessed handle 646 and a protrusive and recessed pipe 647 connected to the

handle; and a scope holder main body 651 and a pin 648. FIG. 221 shows the protrusive and recessed handle 644 and protrusive and recessed pipe 647 connected to the handle.

5 As shown to be partially enlarged in FIG. 218, an outer pipe 652 is adhered to the scope holder main body 651. Further, an inner pipe 653 is adhered to the protrusive and recessed handle 646. The inner pipe 653 can move along an inner face of the outer pipe 652 as a
10 guide. The inner face of the inner pipe 653 is adhered to an external face of a tube 420. Therefore, when the protrusive and recessed handle 646 is moved in the horizontal direction on the drawing surface, the tube 420 moves with respect to the scope holder 628.

15 Similarly, an outer pipe 654 is adhered to the scope holder main body 651. Further, an inner pipe 655 is adhered to the protrusive and recessed handle 646. The inner pipe 655 can move along an inner face of the outer pipe 654 as a guide. The inner face of the inner
20 pipe 655 is adhered to an external face of a tube 439. Therefore, when the protrusive and recessed handle 646 is moved in the horizontal direction on the drawing surface, the tube 439 moves with respect to the scope holder.

25 As shown in FIG. 221, a groove portion 656 is provided at the protrusive and recessed pipe 647, and pin 648 (FIG. 217) is engaged with the pipe.

In a state in which the scope holder 679 and suturing device 3 are mounted on the endoscope 12, suspension can be carried out by utilizing a scope placement site 680 shown in FIG. 223B. At this time, it is preferable that an angle 678 (refer to FIG. 223C) formed by the protrusive and recessed handle 646 be set to 90 degrees with respect to an axle passing through an operating knob 12a of the endoscope 12 such that the protrusive and recessed handle 646 does not interfere with the scope placement site 680 or pole 681.

(Function)

When the protrusive and recessed handle 646 is moved in the horizontal direction on the drawing surface, the tubes 439, 420 move with respect to the scope holder. As shown in FIG. 219 and FIG. 220, the suturing device 3 mounted on the endoscope 12 moves.

(Effects)

The groove portion 656 and pin 648 are engaged with each other, whereby the protrusive and recessed handle 646 does not rotate, and twisting of the tubes 37, 73 as shown in FIG. 222 does not occur. Further, breakage and twisting of the tube 37 or 73 as shown in FIG. 223A is prevented by the outer pipes 652, 654 and the inner pipes 653, 655. As shown in FIG. 223B, when the twenty-first embodiment is carried out, in a state in which the scope holder 679 and suturing device 3 are mounted on the endoscope 12, suspension can be carried

out by utilizing the scope placement site 680.

[Thirtieth Embodiment]

FIG. 224 to FIG. 225B each show the thirtieth embodiment.

5 (Arrangement)

As is obvious from FIG. 224 showing a state in which an endoscope 12 and a suturing device 3 are mounted, a protrusion portion 665 is provided at a jig 664. An inner face 658 of the jig 664 is defined in
10 dimensions for engagement with an outer periphery 659 of a scope fixing portion 666. Further, a cutout portion 660 and a flat face 661 are provided at the jig 664.

(Function)

15 The suturing device 3 and the endoscope 12 are fixed to each other via the scope fixing portion 666 and a hood 603 made of a flexible material fixed thereto. At this time, when the inner face 658 of the jig 664 is fixed so as to be fitted to the outer
20 periphery 659 of the scope fixing portion 666 (FIG. 225A), a flat face 662 of the suturing device and the flat face 661 of the jig 664 are aligned with each other. The cutout portion 660 of the jig 664 is engaged with the scope fixing portion 666. Moreover,
25 the protrusion portion 665 is present in the jig 664, and the endoscope 12 is inserted into the hood 603 at a position at which the protrusion portion 665 enters a

forceps channel 6 of the endoscope 12.

(Effects)

When the endoscope 12 is inserted into or fixed to the hood 603, a fixed angle 657 of the endoscope is
5 determined by using the fixing jig 664. As shown in FIG. 225B, a fixed position of the suturing device 3 with respect to a field of view of the endoscope can be constantly determined.

[Thirty-first Embodiment]

10 FIG. 226 shows the thirty-first embodiment.

(Arrangement)

As is evident from a state in which an endoscope 12 is mounted on a suturing device 3 shown in FIG. 226, the present embodiment is different from the thirtieth
15 embodiment in the following points.

A protrusion portion 663 is present in a scope fixing portion 666. Window portions 683, 684, 685, and 686 are provided in accordance with light guides 8, 9, a CCD camera 10, and an aspirator 11 shown in FIG. 8.

20 (Function)

In the thirtieth embodiment, the endoscope is mounted on the suturing device 3 by using the jig 664. However, in the case of the present embodiment, the protrusion portion 663 of the scope receiver 666 is
25 mounted so as to enter a forceps channel of the endoscope 12.

(Effect)

The endoscope can be mounted at an always precise angle even without using a mounting jig.

[Thirty-second Embodiment]

5 The thirty-second embodiment shown in FIG. 227 is an embodiment of another aspect of the fourteenth embodiment.

(Arrangement)

10 A state in which the endoscope 12 has been mounted on the suturing device 3 is described here. The scope fixing portion 666 can move with tubes 227, 245 being an axle.

(Effect)

15 Fixation of the endoscope 12 and the suturing device 3 becomes more reliable by providing two axes, as compared with a case in which the scope fixing portion 666 shown in FIG. 228 is not stable.

[Thirty-third Embodiment]

20 FIG. 229 to FIG. 231 each show the thirty-third embodiment. The present embodiment is different from the twenty-first embodiment in the following points.

(Arrangement)

25 FIG. 229 shows a field of view F of an endoscope in a state in which a removable needle 441 is mounted on a needle holding member. FIG. 230 shows a field of view F of the endoscope in a state in which the removable needle 441 has been removed from the needle

holding member. As shown in FIG. 231, in the present embodiment, a mark 627 is provided at the outer periphery portion of an end loop cartridge 440 similar to that of the twenty-first embodiment.

5 (Function)

An operation is omitted because the present embodiment is similar to the twenty-first embodiment.

(Effects)

10 In the case of the twenty-first embodiment, when the state shown in FIG. 188A is moved to the state shown in FIG. 188B, the removable needle 441 is moved by touch as to whether or not a needle lock mechanism of the end loop cartridge 440 has been reliably actuated. In contrast, according to the present
15 embodiment, as shown in FIG. 230, the needle lock mechanism is reliably actuated by moving the end loop cartridge 440 to a position at which the mark 627 can be seen. Thus, there is no need to rely on touch.

[Thirty-fourth Embodiment]

20 FIG. 232 to FIG. 234 each show the thirty-fourth embodiment.

(Arrangement)

FIG. 232 shows an outer appearance of the suturing device 3 according to the twenty-first embodiment.
25 This figure shows how a thread 442 is tangled. In contrast, FIG. 233 shows that a second active member 412 is formed in a loop shape. As shown in FIG. 234,

an end loop cartridge 440 is defined in dimensions so as to pass through the second active member 412.

(Effects)

At the second active member 412 shown in FIG. 232,
5 the thread 442 is occasionally tangled. In contrast, in the present embodiment, the second active member 412 is formed in a loop shape as shown in FIG. 233, whereby the thread 422 can be prevented from being tangled.

As shown in FIG. 234, in a state in which the
10 second active member 412 is opened, the end loop cartridge 440 can be attached and detached.

[Thirty-fifth Embodiment]

FIG. 235 shows the thirty-fifth embodiment. The present embodiment is different from the twenty-first
15 embodiment in the following points.

(Arrangement)

As shown in FIG. 235, a suturing device 3 according to the present embodiment is such that a liquid supply circuit 668, a liquid supply tube 667,
20 and a metal base 688 are added to the suturing device 3 according to the twenty-first embodiment.

(Function)

A liquid is supplied from the metal base 688 by using a syringe or the like (not shown).

25 (Effect)

When the suturing device 3 is inserted into the body, even if a field of view is obstructed by adhering

of a mucous liquid, a liquid is supplied from the outside of the body by utilizing a liquid supply circuit, whereby the mucous liquid is removed, and the field of view can be ensured.

5 [Thirty-sixth Embodiment]

FIG. 236A to FIG. 237C each show the thirty-sixth embodiment. The present embodiment is different from the twenty-first embodiment in the following points.

(Arrangement)

10 FIG. 236A shows a needle holding member 434 and a removable needle 441. As in the twenty-first embodiment, a hole 670 and a slit 693 are provided at a distal end of the needle holding member 434. As a fixing portion between the removable needle 441 and the
15 thread 442 is shown in FIG. 236B and FIG. 236C, a knot 689 is used to fix the removable needle 441 and the thread 442 to each other. The removable needle 441 has a hole 691 opening on a rear end face thereof and a hole 690 opening on a distal end tapered face thereof.
20 The hole 690 is greater than the hole 691, and the knot passes through the opening hole 690, but does not pass through the hole 691.

As in a modified example shown in FIG. 237A, a columnar protrusion 699 may be provided at a distal end
25 of the needle holding member 434, and the hole 691 and the slit 692 may be provided at the removable needle 441. As a fixing portion between the removable needle

441 and the thread 442 is shown in FIG. 237B and
FIG. 237C, the knot 689 is used to fix the removable
needle 441 and the thread 442 to each other. The hole
690 is larger than the hole 691, and the knot passes
5 through the hole 690, but does not pass through the
hole 691.

(Function)

In the case of the removable needle 441 shown in
FIG. 236B and FIG. 236C, the knot 689 used for fixation
10 passes through the hole 690, but does not pass through
the hole 691. Thus, even if the thread 442 is pulled
in the left direction on the drawing surface, the
thread 442 does not slip off. This also applies to the
removable needle 441 shown in FIG. 237B and FIG. 237C.

15 When a columnar protrusion 671 of the removable
needle 441 is inserted into the hole 670 of the needle
holding member 434 shown in FIG. 236A, the hole 670 and
the slit 692 broaden, thereby holding the removable
needle 441. The hole 670 is made of SUS420J2, for
20 example, in order to obtain resilient property.

A modified example of FIG. 237A is reverse in
relationship between the hole and the protrusion shown
in FIG. 236A.

(Effects)

25 By using a resilient material, even if the
removable needle 441 and the needle holding member 434
are attached and detached any times, the hole 670 and

slit 692 are not deformed or broadened.

Because the removable needle 441 is designed for a single use, in the case where the removable needle 441 and the needle holding member 434 are attached and detached any times, the durability at the side of the needle holding member 434 is required. In the modified example shown in FIG. 237A, the hole 671 is provided at the removable needle 441 in which the durability is not required so much, whereby the durability is relatively high as compared with that of FIG. 236A even in the case where a combination of the same materials is used.

[Thirty-seventh Embodiment]

(Arrangement)

FIG. 238 shows the end loop cartridge 440 for use in the twenty-first embodiment. FIG. 239 shows a state in which the center axle of a thread lock means 155 shown in FIG. 238 is displaced from the center axle of the end loop cartridge 440.

(Effects)

In the case of the end loop cartridge 440 shown in FIG. 238, a suture thread 156 is fixed by the thread lock means 155. This fixing force quantity is further increased by an edge 673 and an edge 674, and a fixing force quantity when the suture thread is pulled in the direction of an arrow 676 becomes larger than the fixing force quantity of single thread lock means 155. On the other hand, the end loop cartridge 440 according

to the thirty-seventh embodiment is offset in the center axle of the lock means 155 as shown in FIG. 239. Thus, one more edge 675 for engagingly locking the suture thread 156 is provided, so that the fixing force
5 is further increased.

The present invention has been described in conjunction with the preferred embodiments shown in various drawings. Obviously, however, other similar embodiments can be used to realize the same functions
10 as those of the present invention, the above embodiments can be modified, or other embodiments can be added without departing from the spirit and scope of the invention. The present invention is not therefore limited to any single embodiment.

15 For example, it is obvious that each treatment device described above can be used together with a rigid endoscope, trocar, or the like as well as flexible endoscopes. When each treatment device is to be used together with an endoscope, each treatment device can
20 be inserted into the body through a proper lumen extending into the endoscope instead of being arranged outside the endoscope as described above.